

Wireless Sensor Technology for Collecting Surface Electromyography Signals

Yuting Zhu

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Abstract

This main purpose of the research was to develop and manufacture a prototype for a new Wireless Surface Electrode for acquiring surface Electromyography (sEMG) signals from the vastus lateralis muscle from the quadriceps of the knee in real-time.

Initially an extensive literature review was carried out which looked at literature either presented at recognised international conferences or published in journals. The literature review focused on papers from the year 2000 using two keywords, which were 'Wireless' and 'Electromyography'. This showed that the majority of papers had been presented at conferences and published in their proceedings. The literature review showed that there were three main techniques used for wireless transmission with a large variation in the settings for the gain used, filtering and data acquisition of the sEMG signals.

For this research the overall design of the new Wireless Surface Electromyography (WsEMG) Electrodes consisted of two newly designed and developed components: (a) an Electrode Interface Node and (b) a Computer Interface Node.

The wireless link between the two nodes used a ZigBee protocol. The data acquisition was carried out using LabVIEW software to develop a new virtual instrument.

The electrode interface node used an integrated circuit chip from a family programme system on the chip (PSoC[®]). The PSOC[®] chip enable module configuration of the instrumentation amplifier, the low-pass filter, the analogue to digital convertor and it also required a universal asynchronous receiver/transmitter to interface to an XBee[®] transceiver module.

The computer interface node was developed to be a USB dongle to connect to a laptop computer. The USB dongle consisted of another XBee[®] transceiver module and a USB universal asynchronous receiver/transmitter.

The VI was designed and developed using LabVIEW software which allowed for the initial settings for the overall gain and low-pass cut off frequency to be made to the PSoC[®] chip by wireless communication before data acquisition started. The sEMG signal of the muscle was displayed in real time on the laptop and stored as a data file for analysis at a later date.

The subjects used for this research to test the performance of the new WsEMG electrodes and data acquisition were volunteers and for which Ethics Approval was given by the Auckland University of Technology Ethics Committee.

The initial results showed that favourable results were achieved that were comparable to currently used standard wired sEMG electrode systems.

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Statement of Originality

‘I hereby declare that this submission is my own work and that, to the best of my knowledge and belief, it contains no material previously published or written by another person nor material which to a substantial extent has been accepted for qualification of any other degree or diploma of a university or other institution of higher learning, except where due acknowledgement is made in the acknowledgements.’

Yuting Zhu

29th November 2013

Chapter 1

Introduction

1.1 Background

Contractions of skeletal muscles fibres perform movement or force from bioelectrical pulses. Electromyography (EMG) is the term used to describe the study of muscle activity, and is used for measuring the bioelectric pulses. This allows medical professions and researchers to see how a patient's muscles are performing and to make decisions about what can be done to improve the performance of particular muscles.

Formal definitions of EMG include:

“EMG means the recording, registration and evaluation of muscle action potentials”[1]

Or

“An electromyographic (EMG) examination is a functional evaluation of the motor unit. It can assess the location, severity, chronology, and prognosis of injuries, diseases, or other compromises of the motor unit. The motor unit is made up of the anterior horn cell, its axon, and all of the muscle fibers innervated. Some wish to characterize electro diagnosis as synonymous with EMG, and that is historically and conventionally correct, if not correct technically.”[2]

The invasive method of EMG measurement was done by the insertion of needles/wire into the muscles of a patient. This is both painful and unwelcome in many cases. The other practice uses a non-invasive method where electrodes are placed on the surface of the muscle of interest. One of the earliest examples of the study of EMG with the placement of surface electrodes was carried out by Piper [3].

Using these surface electrodes were an improvement to invasive insertion devices but still need to be linked to the data recorder/analyser by a set of wires. This required the patient to be 'wired-up' during testing. The early devices required the wires to be close to the data recorder/analyser, which restricted the usefulness of this technique. As surface electromyography became the customary practice the devices improved, but were still hampered by the endless wires and the back pack that the patient was required to carry for the data to be recorded and analysed.

The changes from wired to wireless surface devices only began to occur when wireless technology developed in other fields such as communication and the military and when this technology became readily available. Wireless devices used for surface Electromyography (sEMG) now included a variety of computerised functions which can report directly to the examiner via computer software to exact features in order to examine the nature of muscular function or dysfunction under investigation.

EMG data received was given in the form of 'wave' patterns or digitised signals, which could be used to diagnose a problem, which needed to be addressed and whether this was within a normal pattern. Early recording required a skilled clinician and frequently the patient did not take part in the conversation as to the problems identified by the procedure. Today with the advancement of technology the clinician can read the muscular activity on the screen of a hand device. This now allows the patient to be able to participate and see the results of muscular activity at the time of the testing. So the patient can be given immediate feed-back in real time and also be encouraged to correctly replicate muscular movements to improve muscular activity if this is the required outcome. Using wireless technology has greatly benefited the clinician and researcher to obtain useful information of how muscles function without the need of a wired system connected to the patient's body.

The following section will cover the various electrodes used today for the collection of electromyography signals.

1.2 Electromyography (EMG) Electrodes

The electrodes are the sensors that measure the bio electrical pulses made by the nerves and muscles. They are either inserted (needle and wire) electrodes or surface electrodes. When electrodes are used individually they are mono-polar and when used in pairs are known as bipolar. Respectively the EMGs readings are acquired as mono-polar or bio-polar configurations [3].

The first principle of designing electrodes is that they must be brought close enough to the muscle under study to pick up the current generated by the muscle movement.

1.2.1 Needle and Wire Electrodes (Invasive)

The most commonly used electrodes for invasive data collection of EMG signals are shown in Figure 1.1 [4].

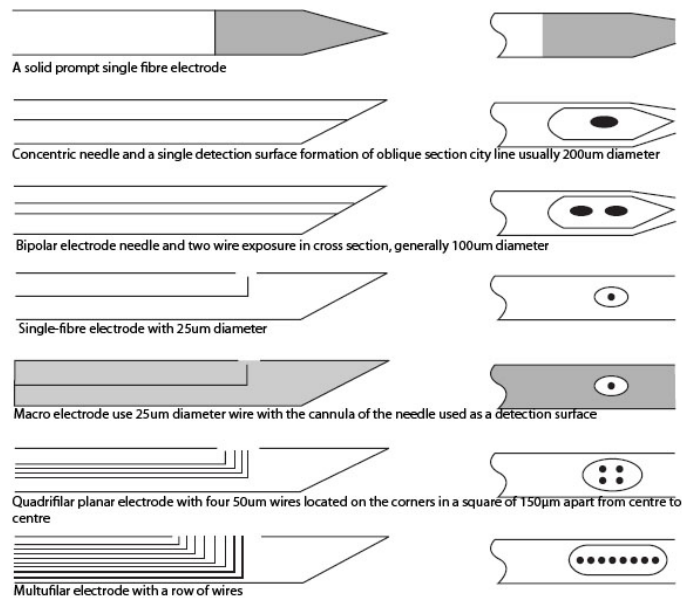


Figure 1.1 – Examples of different needle electrodes

Needle electrodes have changed as a result of improved technologies for testing and recording methodologies. Despite the development and use of surface electrodes, needle electrodes still have a place in the collection of EMG signals.

De Luca et al. [3] described the commonly uses of needle electrodes over surface electrodes, they are:

Motor Unit Action Potential [MUAP] characteristics

Control properties of motor units (firing rate, recruitment, etc.)

Exploratory clinical electromyography

With the development of the wire electrode, De Luca et al. [3]:

Kinesiological studies of deep muscles

Neurophysiological studies of deep muscles

Limited studies on motor unit properties

Comfortable recording procedure from deep muscles

Wired electrodes have led to improvement in muscle measurement knowledge and improved technology has led to an improved understanding of muscle activity. The ability to do further study however, still relies on the agreement of the patient to have a variety of needles inserted into the body; this is uncomfortable and likely to cause some distress to the patient. Whilst the skin surface can be anaesthetised for the needle(s) to be inserted this can cause the ‘deadening’ of the muscles and so no electrical pattern can then be detected. These factors have given pressure for an alternative method to be found to make these readings possible and with less discomfort to the client, which has led to the development and use of surface electrodes.

1.2.2 Surface Electrodes (Non-invasive)

There are two types of surface electrode: **Passive** and **Active**. In each case the electrode head maybe the same but the reading and the recording of the EMG signal is different.

A **Passive Electrode** is shown in Figure 1.2, which has a wider range of reading of muscle activity than the actual focus of the examination. This method gives a less accurate reading as it has greater input impedance. When using passive electrodes the subject will possibly get a small tingling feeling on the skin due to the current produced between the electrode and the surface of the skin.

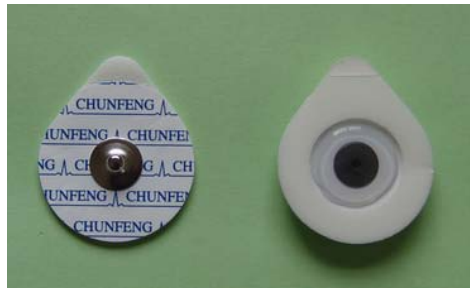


Figure 1.2 – Passive Electrodes

The simplest form of a passive electrode is a silver/silver chloride plate, which adheres to the skin by the application of conductive gel. Impedance between the electrode and the skin can be further reduced by removing any hair and exfoliating the skin before the electrode is attached. Later versions of the passive electrode the conductive gel was part of the electrode. Once a passive electrode has been used for testing purposes it is usually discarded and not used again for future testing. Passive electrodes used today are now all disposable and discarded after use.

The **Active Electrode** shown in Figure 1.3 usually has the ability to reduce the impedance of between the electrode and the skin above the muscle being examined. This is achieved by the inclusion of a high input impedance amplifier in the same housing of the surface electrodes. This arrangement gives the ability to exclude localised impedance and therefore improves the quality of the readings obtained.



Figure 1.3 – Photo of Active Electrode

The impedance again can be further reduced by removing any hair and exfoliating the skin before the electrode is attached. Active surface electrodes have been further developed to eliminate the need for skin preparation and for the conductive gel. These are called ‘dry’ or ‘paste-less’ electrodes.

The active electrode also has its own filtering system using resistances and capacitances within the head of the electrode, which allows the filtering to be coupled close to the skin.

The active electrode has the benefit of being reusable. This requires after use care in terms of storage and hygiene. The multiple uses of the active electrode are also part of its long term unreliability for the following reasons:

1. The constant hygiene cleaning requirements after each and every use means the surface area of the electrode can be vulnerable to minute surface changes which will skew future readings after repeated use.
2. Existing sweat and the erosion of its surface can lead to changes in its electrical properties and also skew later readings.
3. At this time there appears to be no alternative solution to these two problems with active electrodes.

The surface electrode has further described by De Luca et al. [3] and is now mostly used for:

Time-force relationship of EMG signals

Kinesiology studies of surface muscles

Neurophysiological studies of surface muscles

Psychophysiological studies

Interfacing an individual with external electromechanical devices

The greatest advantage of surface electrodes is that they are non-invasive and do not give the patient any discomfort. Moreover, surface electrodes are able to sample a larger volume of muscle but one significant disadvantage is that they can only be used effectively with superficial muscles and they cannot be used to detect signals selectively from small muscles.

Surface electrodes can cause difficulties for the patient when recording movement. The individual is hampered with a multitude of electrodes and wires and so movement maybe difficult or unnatural when recording is taking place. This may cause the patient to make movements which are not their natural movements. The recording may not be of the usual pattern for that movement and hence may not give an accurate diagnosis of the muscular problems for which the testing has been required [5].

The innovation of wireless surface electromyography (WsEMG) technology has greatly improved the ability to measure muscular activity in a more natural and unencumbered way.

1.3 Wireless Surface Electromyography (WsEMG)

Wireless networks are now part of daily lives through smart phones and tablet technology. Creating a wireless sensor network for equipment is feasible and gives the greatest amount of freedom and flexibility to use sEMG in a new free environment to analyse previously seriously restricted abilities.

Wireless technologies offer alternative design solutions for the transmission of complex data communication through such systems as Radio Frequency (RF), Bluetooth and ZigBee etc. In particular, the medical field and the sport and recreation industry stands to benefit widely by substituting wireless systems for wired measurement systems instead of continuing to use the more restricted wired systems.

The advantages of wireless technology is [6]:

1. **Reliability and Mobility** – *the units for wireless are usually in a singular enclosed unit so there are no moving parts.*
2. **Easy Access and Comfort** – *they are easy to use for both patient and clinician with few complicated instructions.*
3. **Low-power consumption** – *Most wireless units now come with advanced batteries or a power source so longer period of use is feasible before recharging is required.*
4. **Real-time processing** – *the recording of data can be completed on site and at the time for the testing without having to wait for this to be completed at a later stage.*
5. **Small size and low-cost** – *recent technology has reduced the sizes of these devices as well as the components used.*

This chapter has shown the development of electromyography from its early days to the current situation of the ability to use modern wireless technology for a medical procedure in some circumstances.

The next chapter will review the literature to show the development of wireless technology related to electromyography. This has led to the development of a new electrode unit which will enhance further the ability of the clinician to diagnose muscle function under set circumstances using this technology.

Chapter 2

Literature Review

This chapter will review the literature on the development of Wireless Surface Electromyography (WsEMG) electrodes and their systems that are used to collect signals from a subject's muscles that are being examined. These signals are then sent to the computer for further analysis at a later date.

As indicated in the first chapter Surface Electromyography (sEMG) is the non-invasive method used to measure the muscle's activity. This is a safe and easy way to record the bioelectrical signal of muscle activity. This has now becoming more widely used for research and clinical applications in many fields for purposes such as rehabilitation programmes, ergonomics and sports performance as well as neurophysiological research [7].

Overall wireless technology provides no wired connections, and is safe with flexible connectivity. It greatly improves resource sharing, is easy to install and has a high mobility factor [6, 8, 9]. The other advantage is that these systems usually use low power levels, thus can be used for a longer period of time before the power source requires renewal [6, 8, 9].

An intensive literature search was carried out, which found that there were a limited number of journal papers published on this topic. But the publications published were mainly found in recognised international conference papers explaining the development of the systems currently developed and used. The search carried out for papers were through recognised databases using the following keywords '*Wireless*' and '*Electromyography*' and limited to papers published since the year 2000. In total 165 papers were found of which 86 were journal papers and the rest were papers presented and then published from recognised conferences. After further extensive examination of these papers a large number were rejected for this literature review due to their unsuitability for the topic being researched i.e. they included using wireless technology for monitoring animal behaviour and many others elements.

The remaining papers used in this literature review were then classified in terms of the wireless protocol used. They were:

1. Radio frequency (RF) (11 papers)
2. Bluetooth (BT) (6 papers)
3. ZigBee (5 papers)

A number of questions were posed to gain the relevant information about each of the systems present in the papers, these were:

- a) What electrode configuration was used i.e. type and material?
- b) Which biosignals were collected with the system?
- c) What amplification and filtering was used and where?
- d) What was the bit resolution of analogue to digital converter (ADC) used?
- e) What type of wireless link was used i.e. type and frequency?
- f) What type of computer interface was used with the wireless system?
- g) What was the sampling frequency used to acquire the sEMG signal?

2.1 Radio Frequency (RF) WsEMG

A radio frequency (RF) signal refers to a wireless electromagnetic signal used as a form of communication, for wireless electronics. Radio waves are a form of electromagnetic radiation identified with radio frequencies ranging from 3 kHz to 300 GHz. RF communication is used in many industries including television broadcasting, radar systems, computer and mobile platform networks, remote control, remote metering/monitoring, and many more such as medical devices.

After an intensive search of the papers only eleven papers were found to be relevant to this research all having being peer reviewed and presented at recognised international conferences. The summary of these papers are presented in Table 2.1 on pages 10 to 12.

Table 2.1 – Summary of the Literature Review for Radio Frequency WsEMG

<i>Paper Title</i>	<i>Authors/Year</i>	<i>Conference or Journal</i>	<i>Electrode Configuration (Type and Configuration)</i>	<i>Type of Biosignals Collected</i>	<i>Amplification and Filters</i>	<i>ADC (Bit Resolution)</i>	<i>Wireless link used and Computer Interface</i>	<i>Sampling Frequency</i>
<i>A Wireless Device for Measuring Hand-Applied Forces'</i>	Tam, W., et al., 2004 [10]	Conference	Not stated.	EMG	Instrumentation amplifier (variable gain). Band-pass filter (100 – 1 kHz).	16-bit	Linx Transceiver System. PCMCIA* card	1 kHz
<i>Design of Implantable Wireless Biomedical Signals Telemetry System</i>	Young-Ho, Y., et al., 2004 [11]	Conference	Not stated.	EMG, ECG**	Not stated	16-bit	Infra-red (Carrier Frequency 37.9 kHz). Micro-processor	8.62 k Hz
<i>Microcontroller-based Wireless Recorder for Biomedical Signals</i>	Chien, C.N., et al., 2006[12]	Conference	Not stated.	EMG, ECG**	Instrumentation amplifier (variable gain). Low-pass filter (variable) with optional High-pass filter.	10-bit	Microcontroller (Carrier Frequency 433.92 MHz). RS-232*** Serial Interface	1 kHz
<i>Development and Evaluation of a Wireless Interface for Inputting Characters Using Laplacian EMG'</i>	Miyazawa, K., et al., 2006 [13]	Conference	Laplacian	EMG	Instrumentation amplifier (variable gain). High-pass filter ($f_c = 100$ Hz).	Not stated	Not stated. Scanning communication system	Not stated

PCMCIA* is Personal Computer Memory Card International Association, ECG** is Electrocardiography, RS232*** is serial port for a personal computer

Table 2.1 (continued) – Summary of the Literature Review for Radio Frequency WsEMG

Paper Title	Authors/Year	Conference or Journal	Electrode Configuration (Type and Configuration)	Type of Biosignals Collected	Amplification and Filters	ADC (Bit Resolution)	Wireless link used and Computer Interface	Sampling Frequency
In situ measurement of playing children by wireless wearable electromyography	Kawakami, G., Y. Nishida, and H. Mizoguchi, 2007 [14]	Conference	Pure active pure silver (Ag) electrode.	EMG	Differential Amplifier (Gain 600). Band-pass filter	10-bit	GFSK* Transceiver module 2.5-2.5 GHz using GSM*** band. USB**** Interface.	1 kHz
Wireless Vestibular Evoked Myogenic Potentials System	Torfs, T., et al., 2007 [15]	Conference	Conventional Ag/AgCl electrodes	EMG	Instrumentation amplifier. High pass filter.	12-bit	Personal body area network (BAN) Not stated.	Not stated
Wireless Transmission of EMG Signal and Analysis of Its Correlation with Simultaneously Acquired Carotid Pulse Wave Using Dual Channel System	Bansal, D., M. Khan, and A.K. Salhan., 2010 [16]	Conference	Ag-AgCl***** electrodes.	EMG	Operational amplifier (gain 500) (100 – 1 kHz).	Not stated.	RF Frequency Modulation Sound port.	8 kHz

GFSK* is Gaussian Frequency-Shift Keying, GSM** is Global System for Mobile Communications, USB**** is Universal Serial Bus, Ag-AgCl***** is Silver/Silver Chloride

Table 2.1 (continued) – Summary of the Literature Review for Radio Frequency WsEMG

<i>Paper Title</i>	<i>Authors/Year</i>	<i>Conference or Journal</i>	<i>Electrode Configuration (Type and Configuration)</i>	<i>Type of Biosignals Collected</i>	<i>Amplification and Filters</i>	<i>ADC (Bit Resolution)</i>	<i>Wireless link used and Computer Interface</i>	<i>Sampling Frequency</i>
Rechargeable wireless EMG sensor for prosthetic control	Lichter, P.A., et al., 2010 [17]	Conference	Not stated.	EMG	Operational amplifier (gain 5) Band-pass filter.	20-bit	Not stated. USB Interface.	Not stated.
Biomedical signal amplifier for EMG wireless sensor system	Rendek, K., et al., 2010 [18]	Conference	Gold (Au) plated.	EMG	Instrumentation amplifier. Band-pass filter (15 – 1 kHz).	16-bit	RF USB Interface.	100 kHz
A Pilot Study on Evaluating Recovery of the Post-Operative Based on Acceleration and sEMG	Zhelong, W., et al., 2010[19]	Conference	Not stated.	EMG	Difference amplifier. Low pass filter, ($f_c = 45\text{Hz}$).	Not stated	Wireless transceiver modules (CC2420) USB Bluetooth dongle.	100 Hz
A Wearable Wireless General Purpose Bio-signal Acquisition Prototype System for Home Healthcare'	Junwei, D., et al., 2012 [20]	Conference	Ag-AgCl electrodes.	EMG, ECG, EEG*.	TI ADS1298 IC (Programmable gain 1-12) Notch filter (50 Hz)	24-bit	RFCC285 Transceiver modules. Serial port.	500 Hz

EEG* is Electroencephalography

2.2 Bluetooth (BT) WsEMG

Bluetooth (BT) was based on the IEEE 802.15.1 standard for wireless personal area networks (WPANs), which are no longer maintained. The BT development and technology is now overseen by the Bluetooth Special Interest Group. This technology is designed to provide reliable, low-power wireless communications over short distances and uses short-wavelength radio transmissions in the Industrial, Scientific and Medical (ISM) band from 2.4 – 2.48 GHz. BT is best known as the primary technology for wirelessly connecting mobile phones with peripheral devices such as wireless headsets. However, BT can be an ideal choice for a wide range of designs such as medical devices.

Only six papers were found to be relevant to this research of which two were from peer review journals and the other four had been presented and published from recognised international conferences. The summary of these papers are presented in Table 2.2 on pages 14 to 16.

Table 2.2 – Summary of the Literature Review for Bluetooth WsEMG

<i>Paper Title</i>	<i>Authors/Year</i>	<i>Conference or Journal</i>	<i>Electrode Configuration (Type and Configuration)</i>	<i>Type of Biosignals Collected</i>	<i>Amplification and Filters</i>	<i>ADC (Bit Resolution)</i>	<i>Wireless link used and Computer Interface</i>	<i>Sampling Frequency</i>
<i>The tremor coherence analyzer (TCA): a portable tool to assess instantaneous inter-muscle coupling in tremor.</i>	Brunetti, F.J., et al., 2004 [21]	Conference	Electrodes using medical-grade stainless-steel.	EMG	Preamplifier with a gain of 20.	8-bit	Bluetooth modules (Blue giga Wrap Thor) Microcontroller	512 Hz
<i>Design and implementation of a wireless (Bluetooth) four channel bio-instrumentation amplifier and digital data acquisition device with user-selectable gain, frequency, and driven reference.</i>	Cosmanescu, A., et al., 2006[22]	Conference	Not stated.	EMG, EKG*	Instrumentation amplifier (Gain 100, 500 and 1000). Band-pass filter (10 – 500 Hz).	10-bit	WBTv42 Bluetooth modules from Wintec Industries. RS232 serial port	2 kHz

EKG* is Electrocardiography

Table 2.2 (continued) - Summary of the Literature Review for Bluetooth WsEMG

<i>Paper Title</i>	<i>Authors/Year</i>	<i>Conference or Journal</i>	<i>Electrode Configuration (Type and Configuration)</i>	<i>Type of Biosignals Collected</i>	<i>Amplification and Filters</i>	<i>ADC (Bit Resolution)</i>	<i>Wireless link used and Computer Interface</i>	<i>Sampling Frequency</i>
Wireless esophageal catheter dedicated to respiratory diseases diagnostic.	Desilets, T., M. Sawan, and F. Bellemare., 2006 [23]	Conference	Platinum ring electrodes.	EMG	Instrumentation amplifier (variable gain). Band-pass filter (35 – 1 kHz).	16-bit	Bluetooth wireless serial port adapter (OEMSPA13i). USB Bluetooth dongle.	1 kHz
Development of a compact-size and wireless surface EMG measurement system.	Wonkeun, Y. and K. Jung., 2009 [24]	Conference	Ag/AgCl electrodes.	EMG	Pre-amplified. Band-pass filter (10 – 500 Hz) and Band-rejection filter (60 Hz).	Not stated.	Bluetooth Not stated.	1024 Hz
Analysis of Right Arm Biceps Brachii Muscle Activity with Varying the Electrode Placement on Three Male Age Groups During Isometric Contractions Using a Wireless EMG Sensor	Ahamed, N.U., et al., 2012[25]	Journal	Active electrodes.	EMG	Pre-amplified. Band-pass filter (5 – 482 Hz).	Not stated	Bluetooth radio modules. SH-SHIM-KIT-004	100 Hz

Table 2.2 (continued) - Summary of the Literature Review for Bluetooth WsEMG

<i>Paper Title</i>	<i>Authors/Year</i>	<i>Conference or Journal</i>	<i>Electrode Configuration (Type and Configuration)</i>	<i>Type of Biosignals Collected</i>	<i>Amplification and Filters</i>	<i>ADC (Bit Resolution)</i>	<i>Wireless link used and Computer Interface</i>	<i>Sampling Frequency</i>
A Wireless sEMG Recording System and Its Application to Muscle Fatigue Detection.	Chang, K.-M., S.-H. Liu, and X.-H. Wu., 2012 [26]	Journal	Ag/AgCl electrodes.	EMG	Instrumentation amplifier (gain 20). Band-pass filter (30 – 1 kHz).	12-bit	Bluetooth modules using chip (BTM-204B) made by CSR Company. Serial port.	2 kHz

2.3 ZigBee WsEMG

ZigBee is a specification for communication in wireless personal area networks (WPANs), like Bluetooth. This technology is designed to be low cost and low powered making it ideal for wireless sensor networks (WSNs) and other low power networks that span potentially large distances. ZigBee builds upon the IEEE 802.15.4 standard, adding extra features such as mesh networking capability with multi-hop functionality and a routing protocol. ZigBee technology does not compete with other technologies such as Bluetooth or Wi-Fi (IEEE 802.11). ZigBee is designed for applications where the data transfer rate is much less important than power efficiency, network size, and the capacity for ad hoc routing. Global operation is in the 2.4GHz frequency band according to IEEE 802.15.4, with regional operation in the 915 MHz (Americas) and 868 MHz (Europe).

After an intensive search of papers only five papers were found to be relevant to this research. One was published in a peer review journal and the other four were papers presented and published papers from recognised international conferences. The summary of these papers are presented in Table 2.3 on pages 18 to 19.

Table 2.3 – Summary of the Literature Review for ZigBee WsEMG

Paper Title	Authors/Year	Conference or Journal	Electrode Configuration (Type and Configuration)	Type of Biosignals Collected	Amplification and Filters	ADC (Bit Resolution)	Wireless link used and Computer Interface	Sampling Frequency
Wireless Head Cap for EOG and Facial EMG Measurements	Vehkaoja, A.T., et al., 2006[27]	Conference	Ag coated reusable electrodes.	fEMG [*] , EOG ^{**}	Instrumentation amplifier (gain 1000). Band-pass filter (10 – 400 Hz).	16-bit	Chipcon's CC2420 ZigBee compliant chip. RS-232 interface.	200 kHz
Design of Wearable, Low Power, Single Supply Surface EMG Extractor Unit for Wireless Monitoring	Sankar, K.A., M. Oishee, and B. Subhasis, 2011 [28]	Conference	Disposable electrodes.	EMG	Instrumentation amplifier (gain 1111). Band-pass filter (10 – 500 Hz).	10-bit	XBee [®] Digimesh 2.4 OEM RF modules. USB Interface.	1 kHz
A portable wireless biometric multi-channel system	Boquete, L., et al., 2012 [29]	Journal	Not stated.	EMG, ECG, EEG, EOG.	Instrumentation amplifier (gain 20). Band-pass filter (0.5 – 1.5 kHz).	12-bit	XBee [®] modules. USB Interface.	400 Hz
A portable multi-channel behavioral state and physiological signal monitoring system	Chung-Ping, Y., et al., 2012 [30]	Conference	Not stated.	EMG, ECG, EEG, EOG.	Not stated.	10-bit	CC2430 Modules. USB to RS-232 convertor.	Approx. 2.8 kHz

fEMG^{*} is Facial Electromyography, EOG^{**} is Electrooculography

Table 2.3 (continued) - Summary of the Literature Review for ZigBee WsEMG

<i>Paper Title</i>	<i>Authors/Year</i>	<i>Conference or Journal</i>	<i>Electrode Configuration (Type and Configuration)</i>	<i>Type of Biosignals Collected</i>	<i>Amplification and Filters</i>	<i>ADC (Bit Resolution)</i>	<i>Wireless link used and Computer Interface</i>	<i>Sampling Frequency</i>
<i>Development of a wearable ZigBee sensor system for upper limb rehabilitation robotics</i>	Cifuentes, C., et al., 2012 [31]	Conference	EMG active electrodes.	EMG	Instrumentation amplifier. Band-pass filter (2 – 500 Hz).	16-bit	ZigBee network consisting of two end devices and one coordinator. Signals stored on micro SD Card, then download to computer.	1 kHz

2.4 Summary of Literature Review Comparison of RF with BT with ZigBee

Table 4 on page 22 shows the results of the seven important questions that were identified at the beginning of this chapter to assist in determining the design of the new wireless system developed in this research. It can be seen that there is little difference in the outcomes when comparing RF, Bluetooth and ZigBee wireless systems used for the collection of EMG signals.

The first factor - the configuration and material used for surface electrodes showed that no clear setup was found throughout all the papers examined. But from known wired setups the commonest setup for the electrodes used the single differential configuration with the electrodes themselves being either dry or pre-gelled made from Ag/AgCl material.

The second factor to be investigated was to identify any other biosignals collected at the same time with wireless systems and being developed in the papers reviewed. It was found that a wide range of biosignals along with EMG were collected which required the setup of the systems presented to be modified to incorporate the biosignals to be obtained. The aim of this research is just to collect sEMG signals and so the setup of the new wireless setup will not have any of the extra features required to collect different biosignals from the body.

The third factor examined was the amplification and filtering of the signals in the overall setup. The findings showed that the most common amplification used an instrumentation amplifier with the filtering of the signal carried out by using a band-pass filter. The band-pass consists of two filters one a low-pass and the other-high pass. There was a wide range of cut-off frequencies found, ranging from 0.5 Hz for high pass to 1.5 kHz for low pass. Also one of the papers showed a notch filter for 60 Hz. This was deemed to be unacceptable for use when examining the frequency content of EMG signals; as the main frequency of an EMG signal lies between 0 to 500 Hz, with the dominance being in the 50 to 150 Hz range [32]. The new design of a system presented in this research incorporated an instrumentation amplifier with a band-pass filter.

The fourth factor investigated was the bit-resolution of the analogue to digital conversion of the signal and it was found in the range from 8-bit to 24-bit. This factor is important as a low bit resolution will give a poor picture of the signal being collected whereas a higher bit resolution gives a better picture of the signal but is major problem in terms of the transfer rate of the signal being acquired. So a balance between the transfer rate and bit resolution of ADC needs to be found [33].

The fifth point examined in all the papers reviewed was the wireless transmission standard to use, whether to use RF, Bluetooth or ZigBee. The setup for this research proposed to use the ZigBee protocol as this was the fastest developing protocol used in the world of wireless transmission of data for miniaturised standalone wireless devices.

The sixth point reviewed was how the wireless system was connected to the computer for displaying information and the data storage of the signals being collected. It was found that this was achieved by either using the RS232 serial port using or a USB port. The wireless setup of the system being developed for this research will use a USB port with a newly developed dongle.

The last point reviewed from the papers examined was sampling the frequency of the systems used to acquire the EMG signals. The values of the sampling frequencies had a wide range from as low as 400 Hz and as high as 200 KHz. This required further research and examining the useful frequency content of EMG signals. It was found that the optimum frequency should be set up at a value no less than 1 kHz [34].

Table 2.4 – Comparison of the Three Wireless Systems Examined

Questions	Radio Frequency	Bluetooth	ZigBee
What electrode configuration was used i.e. type and material?	There was no clear common electrode configuration used and material used.	There was no clear common electrode configuration used or material.	There was no clear common electrode configuration used, or material used.
Which biosignals were collected with the system?	The other biosignals collected with systems were ECG and EEG.	The other biosignals collected with these systems were electrocardiography (EKG) signals.	The other biosignals collected with this system were fEMG, ECG, EEG and EOG.
What amplification and filtering was used and where?	Any amplification of the signals was commonly amplified by instrumentation amplifiers with band-pass filtering.	Any amplification of the signals was commonly amplified by instrumentation amplifiers with band-pass filtering.	Any amplification of the signals was commonly amplified by instrumentation amplifiers with band-pass filtering.
What was the bit resolution of analogue to digital converter (ADC) used?	The most commonly used bit resolution of the analogue digital conversion was 16-bit but was as low as 10-bit and as high as 24-bit.	The most commonly used bit resolution for the analogue digital conversion ranged from 8-bit to 16-bit.	The most commonly used bit resolution for the analogue digital conversion was as low as 10-bit and as high as 16-bit with 16-bit the most common.
What type of wireless link used i.e. type and frequency?	The type of wireless links using RF frequencies varied from infra-red links to sound waves.	The types of wireless links used were different commercially available Bluetooth transceiver modules.	The type of wireless link used was a ZigBee industry compliant transceiver such as the XBee® modules.
What type of computer interface was used with wireless system?	The most commonly used computer interface to the wireless system was the computer serial port or USB port.	The most commonly used computer interface used a RS232 serial port or the USB port with a Bluetooth dongle.	The most commonly used computer interface for this wireless system was serial RS232 port or a USB dongle.
What was the sampling frequency used to acquire the sEMG signal?	The sampling rate for the data collection of the signals varied greatly from 500 Hz up to several values in kHz's.	The sampling rate for the data collection of the signals varied greatly from 512 Hz up to 2 kHz.	The sampling rate for the data collection of the signals varied greatly from 400 Hz up to 2.8 kHz.

This chapter summarised the literature review for various types WsEMG technology such as (a) RF, (b) Bluetooth and (c) ZigBee that have been presented at conferences and then published as part of the conference papers; or published in journals. It has shown that the majority of papers published have been presented at conferences with very few published in journals. This has shown that WsEMG technology is in its infancy and has a long way to go before it can be recognised as a credible alternative technology that can be used in the data collection of sEMG signals.

The next chapter will present the methodology used in the design, development and creation of the new WsEMG electrodes used in this research.

Chapter 3

Methodology in the Development of Wireless Surface Electrodes

This chapter will discuss the methodology used for the design, development and building of the new Wireless Surface (WsEMG) Electrodes used in this research, and the data collection of sEMG signals from the *vastus lateralis* muscle of the quadriceps.

Chapter 2 in the literature review it was found that there were three main techniques used for the wireless link between sEMG electrodes and the computer. These were:

- RF
- Bluetooth
- ZigBee

For the purposes of this research ZigBee was chosen as the wireless link for the transmission of the sEMG signals between the electrodes and the laptop computer used for data storage purposes.

This chapter will discuss the methodology used in the design and development of the electrodes only from the initial concept to the final design and build of the WsEMG electrodes to be used.

3.1 Concept and Block Diagram of WsEMG Electrodes

The proposed block diagram for the system is shown in Figure 3.1 and incorporates two separate nodes. The sensor node will be placed on the subject's body and the other a USB dongle node is connected to the laptop computer for receiving and storing the data.

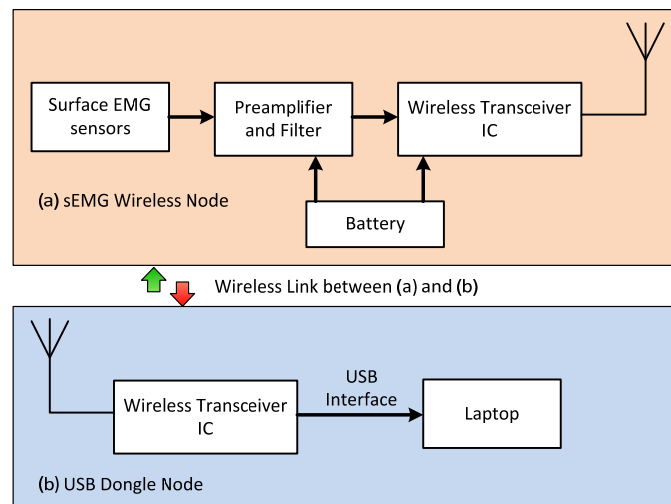


Figure 3.1 – The Proposed Block Diagram for the Design/Build of WsEMG Electrodes

The detail of the literature review and current trends in wireless technology influenced the design and development of the systems used for the WsEMG electrodes. The detailed block diagram Figure 3.2 shows the necessary components needed to be considered in the final system built. The main component used was the Cypress PSoC[®] chip, which incorporated a number of features necessary for the design of the WsEMG electrodes to be used in this research.

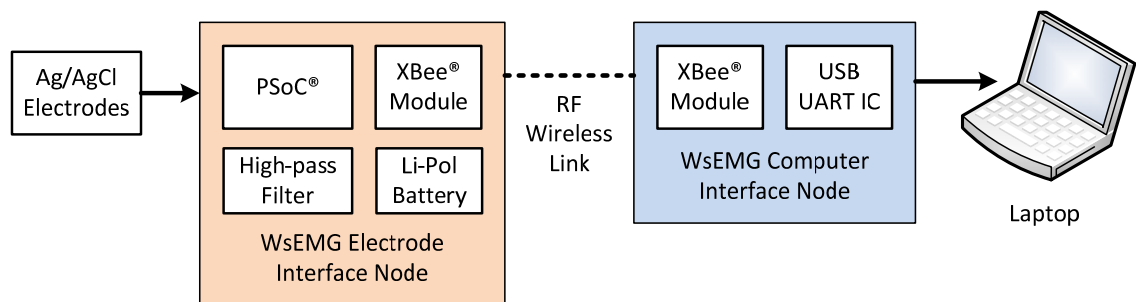


Figure 3.2 – The Components Used for the WsEMG Electrodes

This new WsEMG system has been split into two different modules and is covered in sections:

3.2 WsEMG electrode interface node

3.3 WsEMG laptop computer interface node

3.2 WsEMG Electrode Interface Node

The *WsEMG electrode interface node* made the connection between the surface Ag/AgCl surface electrode and the RF wireless link, which consists of four main components and will be covered in sections:

- 3.2.1 Programmable System-on-Chip (PSoC[®])
- 3.2.2 High-pass Filter
- 3.2.3 XBee[®] Transceiver Module
- 3.2.4 Lithium-ion Polymer (Li-Pol) Battery and Charger

3.2.1 Programmable System-on-Chip (PSoC[®])

The main component for the new WsEMG electrode system was the CY8C29466-24PVXA integrated circuit chip from the family of PSoC[®] 1 made by the Cypress, Semiconductor Corporation, USA, see Appendix A for the datasheet.

The PSoC[®] chip has integrating configurable analogue and digital peripheral functions which are supported by an integrated development environment (IDE) PSoC[®] Designer™ to programme the chip with the following functions:

- Instrumentation Amplifier plus programmable gain amplifier
- Low-pass Filter
- Analogue Digital Convertor (ADC)
- Universal Asynchronous Receiver/Transmitter (UART) interface to the XBee[®] transceiver module

The required configurable module layout box for the PSoC[®] integrated circuit chip for the WsEMG system is shown in Figure 3.3 inside the yellow shaded box.

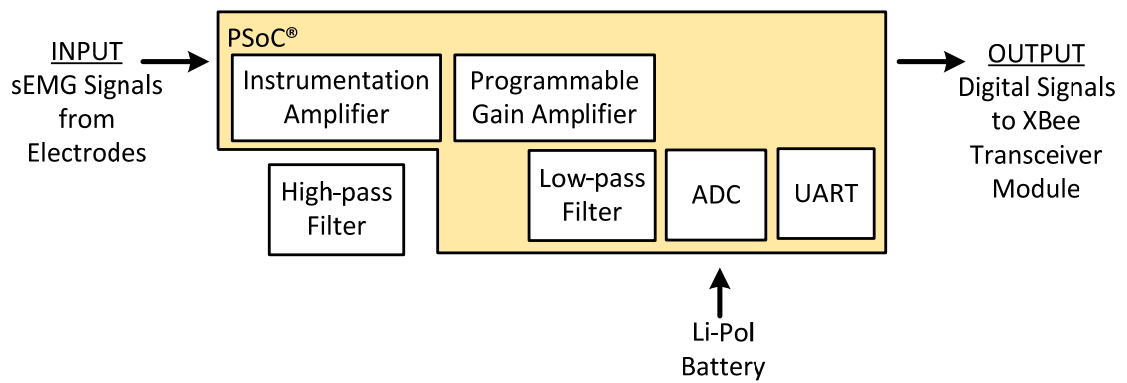


Figure 3.3 – The PSoC® Individual Modules that are required to be configured

Using the PSoC® chip has made the wireless electrode interface mode more flexible. The configuration for the gain and filtering is easily done in terms of coding and does not require any changes in the physical hardware components.

There are six modules which are required to be configured and coded on the PSoC® CY8C29466-24PVXA chip for the WsEMG electrode interface. These are covered in sections:

- 3.2.1.1 Instrumentation Amplifier
- 3.2.1.2 Programmable Gain Amplifier
- 3.2.1.3 Low Pass Filter
- 3.2.1.4 Analogue Digital Convertor (ADC)
- 3.2.1.5 UART
- 3.2.1.6 24-bit timer

To be able to configure the PSoC® chip as required for the WsEMG, PSoC® Designer™ software is required, which has its own Integrated Design Environment (IDE). The IDE allows the user to be able to customise the integrated circuit to meet specific application requirements. The PSoC® Designer™ has the following subsystems:

The PSoC[®] Designer[™] IDE workspace shown in Figure 3.4 area has a number of active windows that differ depending on the functionality of the subsystem are in. These are:

- Chip-Level Editor
- Code Editor
- Build Manger
- Debugger

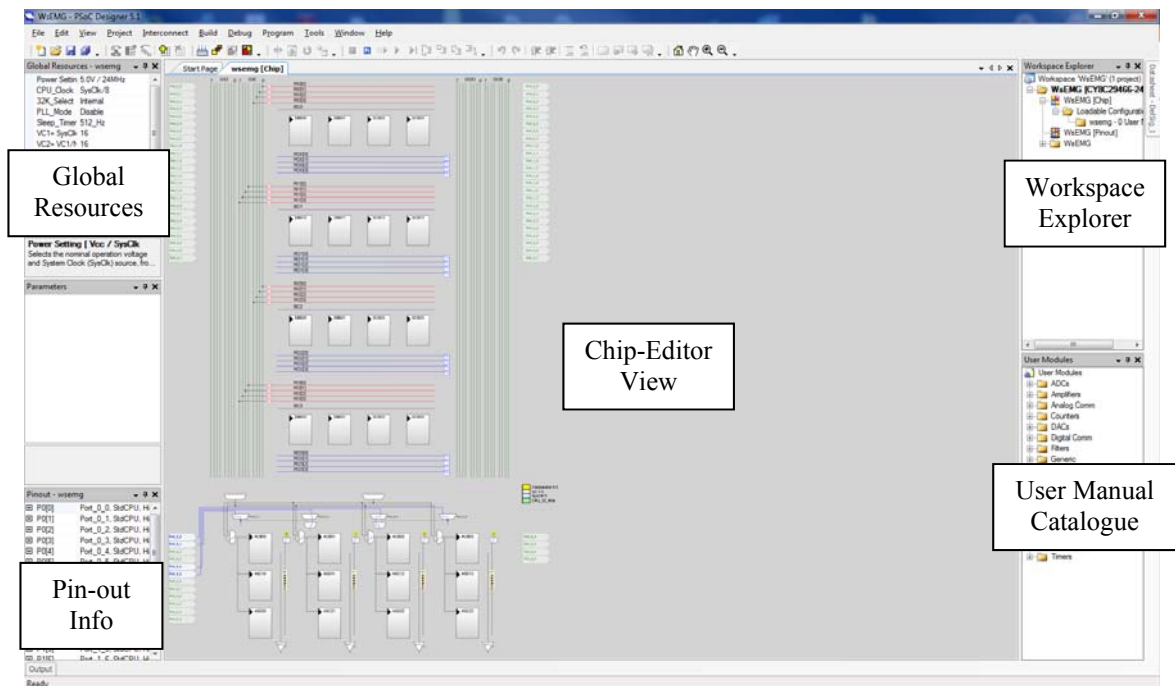


Figure 3.4 – The IDE Workspace for the PSoC[®] Designer[™]

The **Chip-Level editor** which is the main view of the IDE shows the diagram of the resources available on the CY8C29466-24PVXA chip to be selected and is shown in detail in Figure 3.5. The blocks types available are split into either digital or analogue and the interconnections to the pins of the chip.

The **Code Editor** is a full featured text editor designed for editing and assembling the C code in the project. The C code is the application code that is downloaded on the PSoC[®] chip for the modules selected from the Chip Editor.

The **Build Manger** is the utility that controls the various parts of the build process including the compiler, assembler and linker. It also manages the process of building the project and preparing the download to the PSoC[®] chip.

The **Debugger** this has multiple windows that allow interaction and observe the code execution on the PSoC[®] chip.

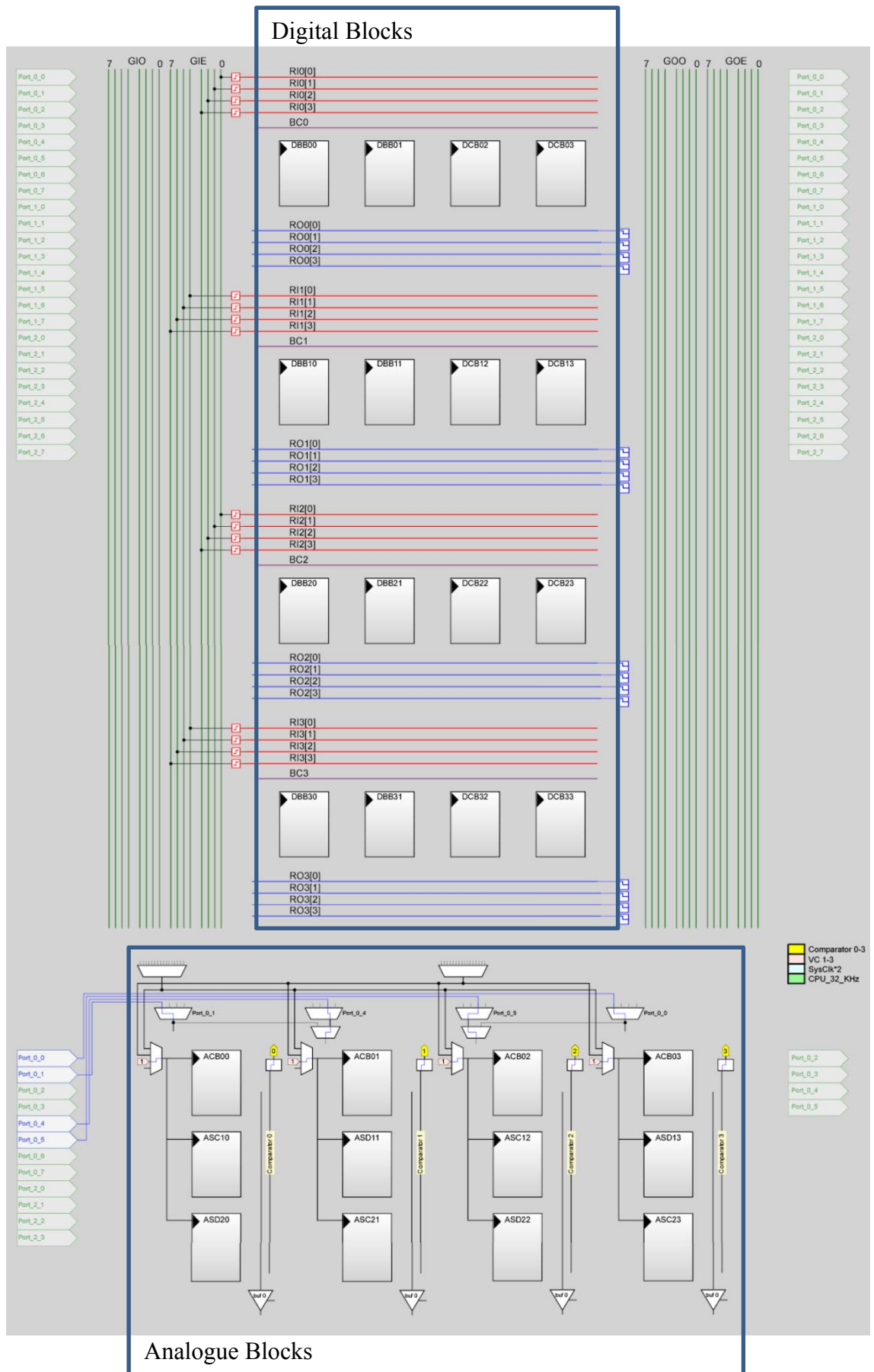


Figure 3.5 – The Detail View of the Chip Editor Window for CY8C29466-24PVXA chip of IDE Workspace

3.2.1.1 Configuration of Instrumentation Amplifier

The CY8C29466-24PVXA chip offers analogue module blocks for configuration of the instrumentation amplifier to collect the sEMG signals from the surface electrodes, and was selected for the following points:

- Low Noise
- Low Nonlinearity
- Simple Gain Selection
- Adequate Bandwidth

The instrumentation analogue module blocks on the PSoC[®] chip being used have the following features:

- User-programmable gain from 2 to 16 with a two op amp topology
- User-programmable gain up to 93 for the three op amp topology
- High impedance differential inputs
- Single-ended output
- Selectable reference with the two op amp topology

The instrumentation amplifier with the three op amp topology has been chosen as it had excellent common mode rejection ratio (CMRR) and a wide dynamic range. The schematic of the three op amp topology is shown in Figure 3.6.

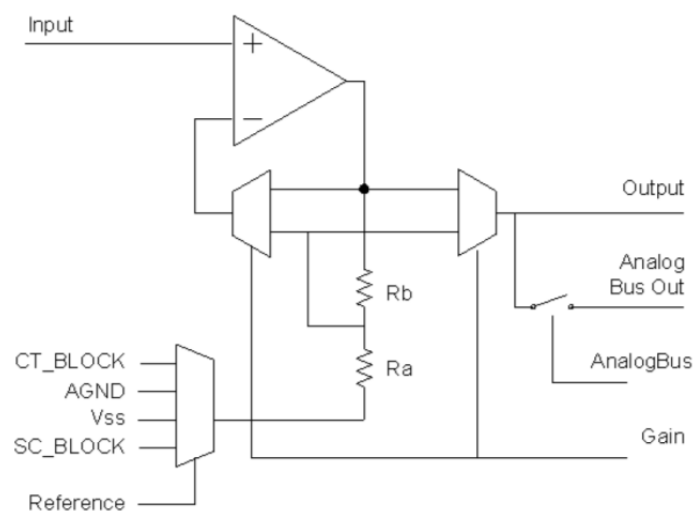


Figure 3.6 – Circuit diagram for the Instrumentation Amplifier (three op amp topology)

Three analogue block modules were required to implement the instrumentation amplifier on the IDE is shown in Figure 3.7 by three red coloured boxes, labelled as:

- a. INSAMP NON_INV
- b. INSAMP INV
- c. INSAMP CONVERT

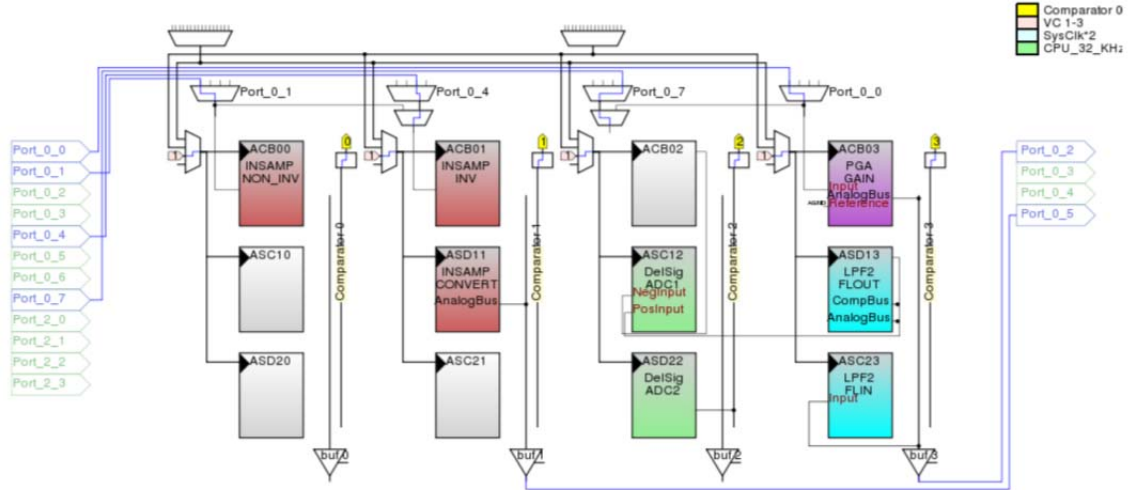


Figure 3.7 – The Analogue Modules used to configure Analogue Elements of the WsEMG System on the PSoC®

The output voltage of INV and NON_INV block are given by Equations 3.1 and 3.2 respectively.

$$V_{out\ INV} = V_{CM} + \left(1 + \frac{R_b}{R_a}\right) \left(\frac{V_{IN+} - V_{IN-}}{2}\right) \quad \text{Equation 3.1}$$

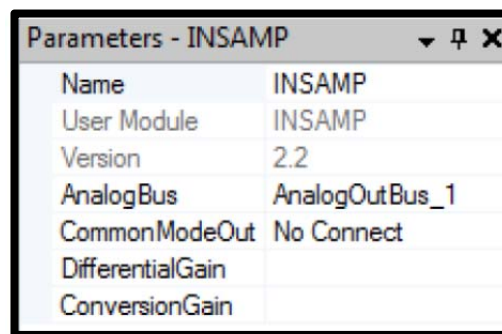
$$V_{out\ NONINV} = V_{CM} - \left(1 + \frac{R_b}{R_a}\right) \left(\frac{V_{IN+} - V_{IN-}}{2}\right) \quad \text{Equation 3.2}$$

From Figure 3.7 the output of block INV drives the capacitor C_b input of CONVERT and the output of block NON_INV drives the capacitor C_a input of CONVERT. The sign of the C_b input is fixed by block topology to be negative and the sign of the C_a input is set in the User Module firmware to be positive. The capacitors C_a and C_b have identical values; so the conversion of the continuous time block outputs is the differential and the output of CONVERT is given by Equation 3.3.

$$CONVERT = V_{AGND} + (V_{IN+} - V_{IN-}) \left(1 + \frac{R_a}{R_b}\right) \frac{C_a}{C_b} \quad \text{Equation 3.3}$$

The available resistor ratios for R_b and R_a set the useful gain range of the input stage to values between 1.0 and 48.0. Conversion gains in the switched capacitor block can be between 0.032 and 1.9375 (i.e. 1/32 to 31/16). This yields a large number of useful gain settings between 1.0 and 93. Differential Gain and Conversion Gain are set independently by the user as parameters in PSoC[®] Designer[™] and may be changed at run time through the SetGain Application Programming Interface (API) function.

The input of the instrumentation INV and NON_INV inputs were connected to port_0_1 and port_0_4 respectively see Figure 3.7. The output of the instrumentation amplifier is placed on the analogue column output bus using the enable selection of the AnalogBus module parameter see Figure 3.7. The AnalogBus module parameter was set to the AnalogOutBus_1 and the other setting for the parameter was set in the API with the CommonModeOut is set to No Connect. Figure 3.8 shows the setting of the module parameters.



Parameters - INSAMP	
Name	INSAMP
User Module	INSAMP
Version	2.2
AnalogBus	AnalogOutBus_1
CommonModeOut	No Connect
DifferentialGain	
ConversionGain	

Figure 3.8 – The Setting of Instrumentation Amplifier in the API window

3.2.1.2 Configuration of Programmable Gain Amplifier

The Programmable Gain Amplifier used on the PSoC[®] has following features:

- Thirty-three user-programmable gain settings with a maximum gain of 48.0
- High impedance input
- Single-ended output with selectable reference

The Programmable Gain Amplifier circuit diagram is shown in Figure 3.9 and only required one analogue block module to be implemented on the IDE, shown in Figure 3.7 by the purple coloured box, labelled as PGA GAIN.

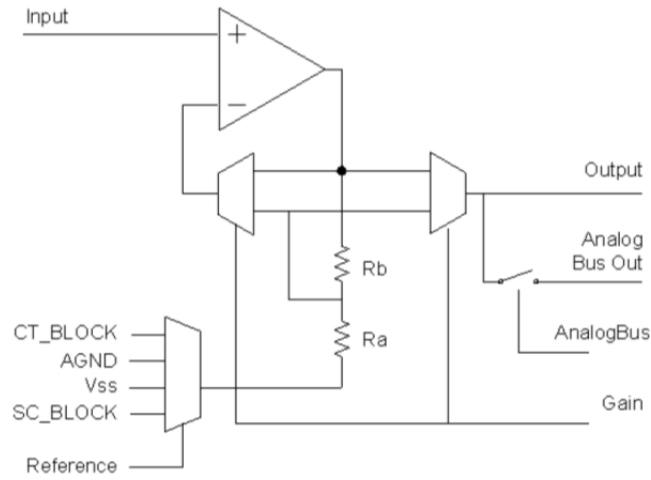


Figure 3.9 – Circuit diagram for the Programmable Gain Amplifier

This module amplified an internal or externally-applied signal. This signal could be referenced to the internal analogue ground, Vs or other selected references. The gain was set by programming the selectable tap in a resistor array and the feedback tap in a continuous time analogue PSoC[®] block. The output voltage was determined by using two equations. For a gain greater than or equal to one, the top resistor string was connected to the op-amp output and the resistor tap was connected to the inverting input of the op-amp. The gain was calculated using Equation 3.4.

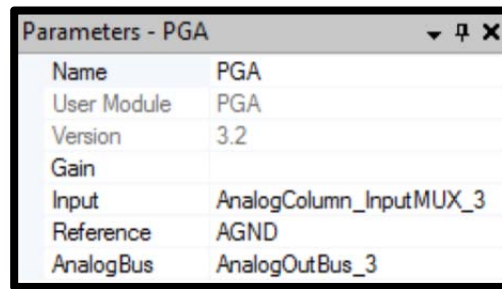
$$V_{out} = (V_{IN} - V_{GND}) \left(1 + \frac{R_b}{R_a} \right) + (V_{GND}) \quad \text{Equation 3.4}$$

For the gain of less than one, the op-amp was set as a voltage follower and the user module output was selected at the resistor tap. The gain is calculated using Equation 3.5.

$$V_{out} = (V_{IN} - V_{GND}) \left(\frac{R_a}{R_a + R_B} \right) + (V_{GND}) \quad \text{Equation 3.5}$$

The input to the programmable gain amplifier were driven by the outputs of the adjacent PSoC[®] blocks and the analogue column input multiplexer and was set to AnalogColumn_InputMUX_3. The gain of the PGA was referenced to AGND (on-chip

analogue ground). The AnalogBus parameter was set to AnalogOutBus_3, which was off pin_0_2. The API settings are shown in Figure 3.10.



Parameters - PGA	
Name	PGA
User Module	PGA
Version	3.2
Gain	
Input	AnalogColumn_InputMUX_3
Reference	AGND
AnalogBus	AnalogOutBus_3

Figure 3.10 – The Setting of Programmable Gain Amplifier in the API window

3.2.1.3 Configuration of Low Pass Filter

The PSoC[®] CY8C29466-24PVXA only allowed for a two-pole low-pass filter to be configured using the IDE. So when a band pass filter was used for the WsEMG a high-pass filter needed to be used and configured alongside the chip as shown in Figure 3.3. This was required because there were no high-pass filter module available on the chip. The low-pass features on the PSoC[®] had the following attributes available:

- User-programmable gain
- User-programmable corner frequency and damping ratio with no external components
- Filter corner-frequency stability directly derived from clock accuracy
- Filter sampling rates to 1.0 MHz

This module implemented a general purpose second order state variable low-pass filter. The corner frequency and damping ratio are functions of the clock frequency and the ratios of the selected capacitor values. This could be implemented on any classical all-pole filter configuration (Butterworth, Bessel and Chebyshev). The corner frequency could be set very accurately or adjusted by controlling the sample rate clock.

The low-pass filter is shown in Figure 3.11 and it required only two analogue block modules to be implemented on the IDE, shown in Figure 3.7 by the light blue coloured box, labelled as:

- a. LPF2 FLIN
- b. LPF2 FLOUT

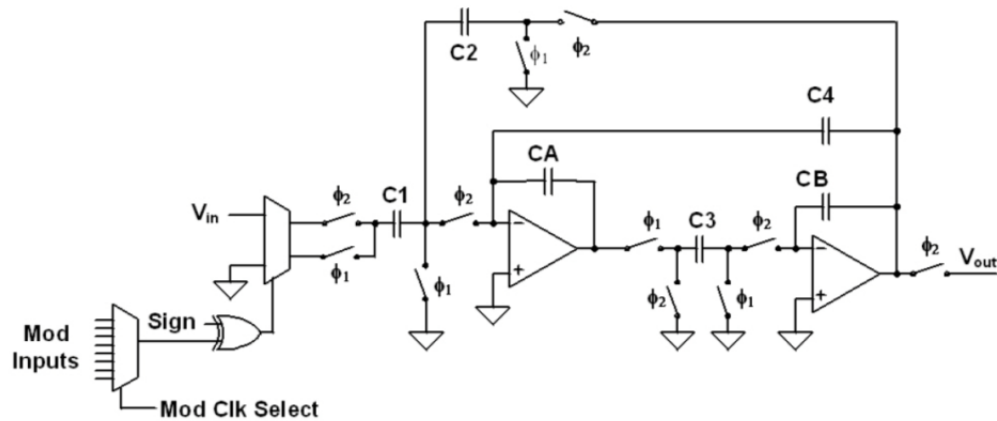


Figure 3.11 – Circuit diagram for Two-Pole Low Pass Filter

The PSoC[®] Designer[™] provided a filter design wizard to automate the procedure for the two-pole filters show in Figure 3.12. In the wizard all that needed to be activated was to select the cut-off frequency and sampling rate of the frequency and filter type. It will then generate the required parameters for the research. The filter configuration for the WsEMG system was a Butterworth filter with a cut-off frequency of 1 kHz.

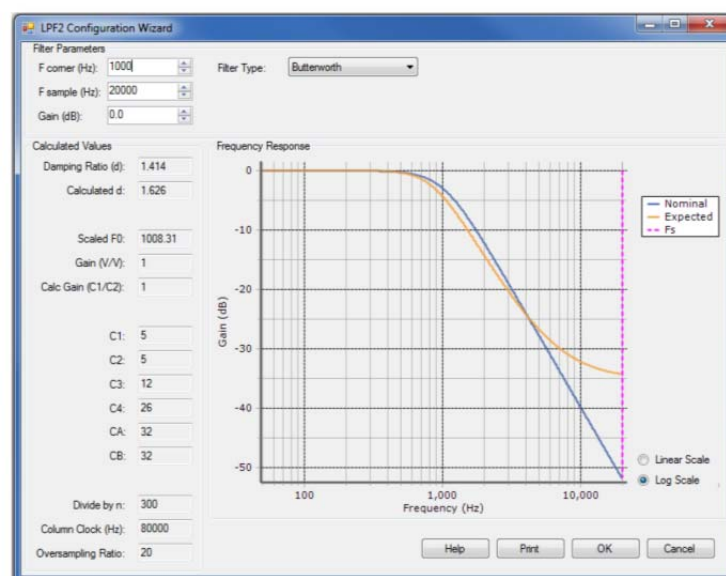
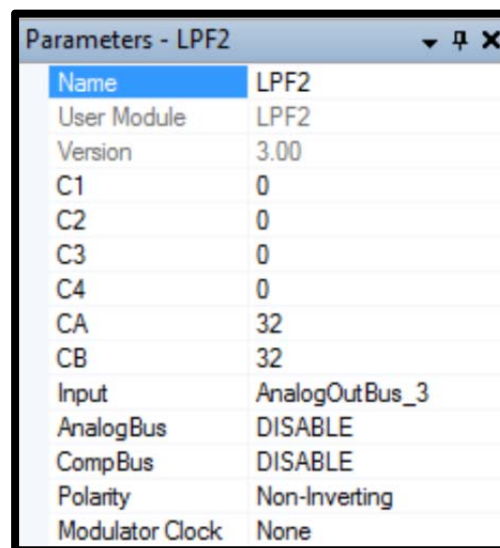


Figure 3.12 – The output from the Filter Design for a Butterworth Low-Pass Filter with a cut-off of 1 kHz

The inputs to the filter are driven by the output of the PGA module. The AnalogBus is was not been connected to this module. The CompBus which was a FLOUT block comparator output needed to be routed to the input bus of the digital PSoC[®] blocks or to an interrupt. This was also not connected for this module. Polarity is the parameter that determines the polarity of the output relative to the input, in this research it was been sets to Non-inverting. The Modulator Clock was used to connect the polarity control in the A input of the input block (FLIN). For this research it had been set to none. Figure 3.13 shows the API settings for the two-pole low-pass filter.



Name	LPF2
User Module	LPF2
Version	3.00
C1	0
C2	0
C3	0
C4	0
CA	32
CB	32
Input	AnalogOutBus_3
AnalogBus	DISABLE
CompBus	DISABLE
Polarity	Non-Inverting
Modulator Clock	None

Figure 3.13 – The Two-Pole Low-Pass Filter settings in the API window

3.2.1.4 Analogue Digital Convertor (ADC)

The CY8C29466-24PVXA chip offers analogue and digital module blocks for the configuration of an ADC. The ADC used was a Delta Sigma ($\Delta\Sigma$) ADC, which was ideal for converting analogue signals over a wide range of frequencies, from DC to several megahertz. Basically, these converters consisted of an oversampling modulator followed by a digital/decimation filter that together produced a high-resolution data-stream output.

The ADC on the PSoC[®] has the following features:

- 6-bit resolution with 32X oversampling to 14-bit resolution with 256X oversampling
- Data in unsigned or signed 2's complement formats
- Maximum sample rates of 65,500 sps at 6 bit resolution, 7812 sps at 14-bit resolution

The ADC circuit diagram is shown in Figure 3.14 and it required only two analogue block modules to activate the input to the ADC. This would need to be implemented on the IDE, and is shown in Figure 3.7 as green coloured boxes, labelled as:

- DelSig_ADC1
- DelSig_ADC2

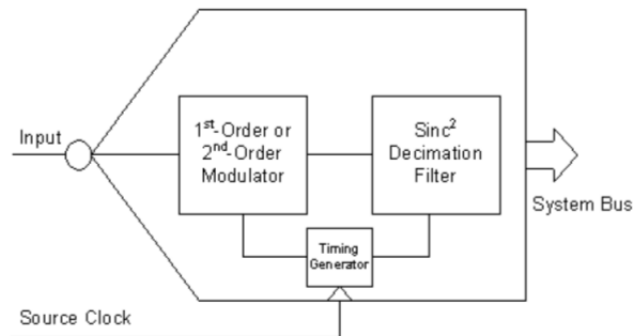


Figure 3.14 – Circuit diagram for the Delta Sigma (DΣ) ADC

Also two digital block modules to act as the output from the ADC were required to be implemented on the IDE. These are shown in Figure 3.15 as green coloured boxes, labelled as:

- DelSig PWMLSB
- DelSig PWMLSB Output

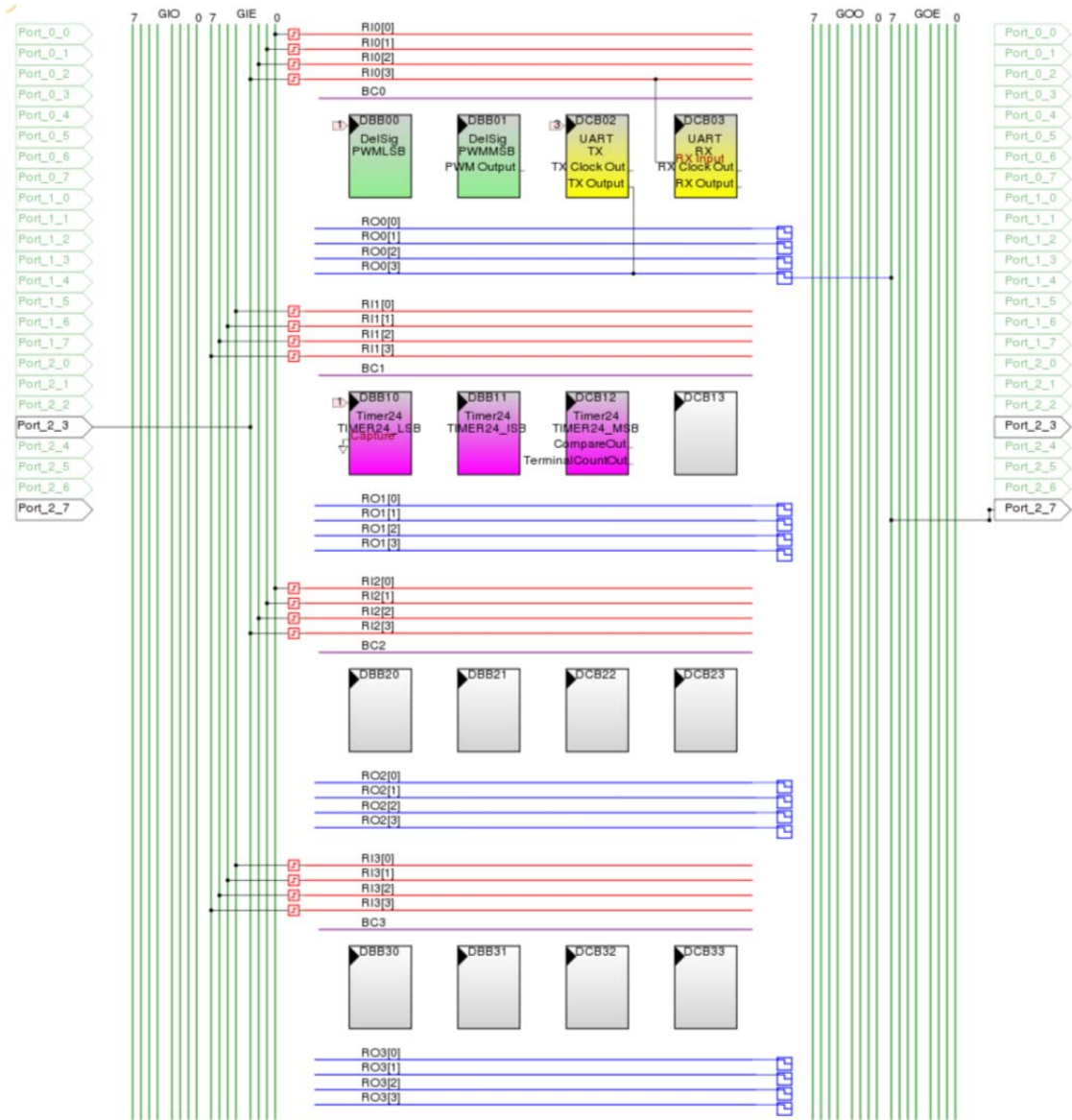


Figure 3.15 – The Digital Modules used to configure Digital Elements of the WsEMG System on the PSoC[®] on the IDE

The output rate was determined by dividing the data by 4 to get the 1-bit over sample rate and then divided by the decimation rate to get the final sample rate by using Equation 3.6.

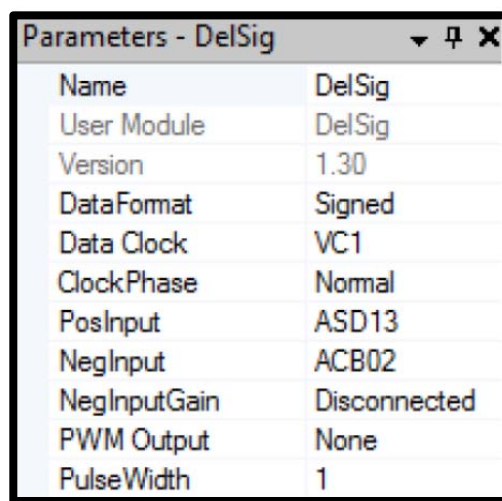
$$\text{Sample Rate} = \frac{\text{Data Clock Frequency}}{4 \times \text{Decimation Rate}} \text{ samples/second} \quad \text{Equation 3.6}$$

It would use a 12-bit DelSig ADC in the research. The decimation rate for the 12-bit ADC is 128. So if the research required 1000 samples per second, the data clock frequency could be calculated using Equation 3.7.

$$\begin{aligned} \text{Data Clock Frequency} &= \text{Sample Rate} \times 4 \times \text{Decimation Rate} \\ &= 1000 \times 4 \times 128 = 0.512 \text{ MHz} \end{aligned} \quad \text{Equation 3.7}$$

As the maximum range of the signals was required, so it was chosen to the RefMux parameter to $(V_{DD}/2) \pm (V_{DD}/2)$ with the range for input is from 0 to 3.3V. Since the 12-bit ADC was chosen, so total will be $2^{12} - 1$ which is 4095 samples, so each sample will be 0.00080586 V.

The data format parameter was set to signed data because it gave a range in the value from -2^{n-1} to $+2^{n-1} - 1$. The Data clock parameter was set to VC2 which had been set to 0.533 MHz. The sample rate work out was set at 1048 which is close to 1000 samples per second. The clock phase was set to normal. PosInput was set to the ASD13 block which was set to the output block of the low-pass filter. The NegInput was set to the ACB02 block since that block would have no module setting. The NegInputGain was set to disconnected, as this function would not be required. The PWM output was set to none. The Pulse Width was set to 1. The research would not be using the PWM and the NegInput so no settings were configured. Figure 3.16 shows the parameters settings.



Name	DelSig
User Module	DelSig
Version	1.30
DataFormat	Signed
Data Clock	VC1
ClockPhase	Normal
PosInput	ASD13
NegInput	ACB02
NegInputGain	Disconnected
PWM Output	None
PulseWidth	1

Figure 3.16 – The ADC settings in the API window

3.2.1.5 Universal Asynchronous Receiver/Transmitter (UART)

The UART module provided by the PSoC® has following features:

- Asynchronous receiver and transmitter
- Data-format compliant with RS-232 serial-data format
- Burst rates up to 6 M bits/second
- Data framing consists of start, optional parity, and stop bits

The UART module is 8-bit that supports data format serial communications over two wires. The received and transmitted data format includes a start bit, optional parity, and a stop bit; see Figure 3.17 for the block diagram of UART. Two digital block modules were required to be implemented on the IDE, and all shown in Figure 3.15 as the yellow coloured boxes, labelled as:

- a. UART TX
- b. UART RX

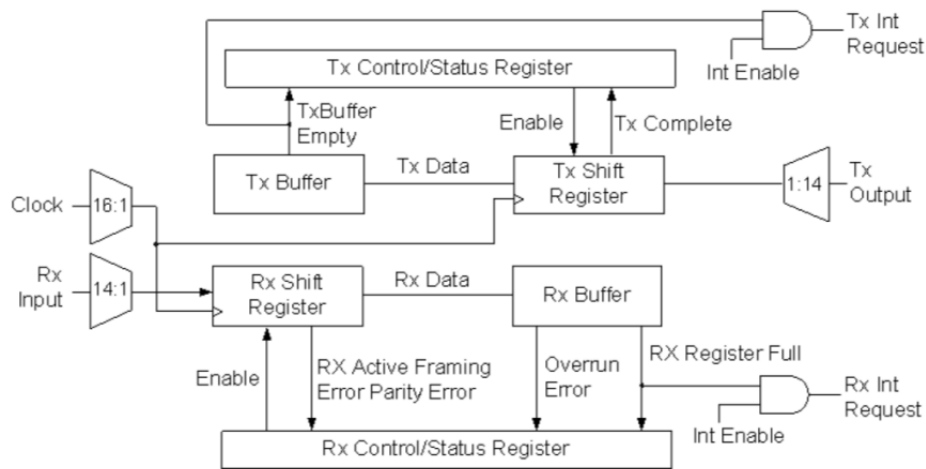


Figure 3.17 – Block diagram for the UART

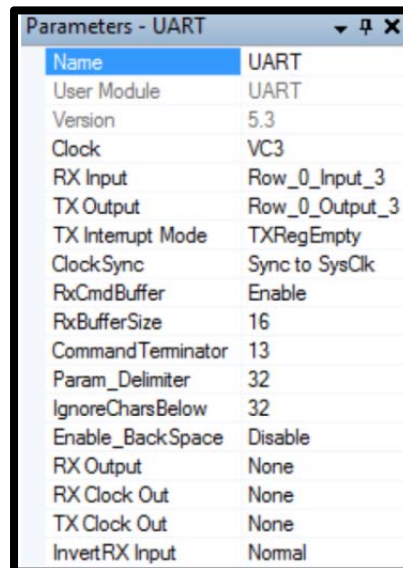
The UART User Module implemented a serial transmitter and receiver. The UART mapped onto the two PSoC® blocks which were designated TX and RX. The TX PSoC® block gives transmitter functionality and the RX PSoC® block gives receiver functionality. The RX and TX blocks operate independently. Each had its own Control and Status register, programmable interrupts, I/O, Buffer register, and Shift register. They share the same enabled, clock, and data format. Setting the Enable bit in the RX Control and TX Control registers enables the UART to operate. Enabling and disabling

was performed using the API provided functions. The UART User Module clock was shared by both the RX and TX components. The clock frequency selected had to be eight times the frequency of the required data bit rate. Each received or transmitted data bit requires eight input clock cycles. The data received and transmitted was a bit stream that consisted of a start bit, eight data bits, an optional parity bit, and a stop bit.

The clock setting for the UART module was set to VC3. Since the XBee[®] baud rate was set to 115200 bps, it needed to match the baud rate for the PSoC[®] UART module to 115200 bps as well. The clock rate was set to eight times the desired bit rate. One data bit was received or transmitted every eight clock cycles. The VC3 was set to the system clock to divide by 27 so the baud rate was found using Equation 3.8.

$$\text{baud rate} = \frac{24 \text{ MHz}}{27 \times 8} = 512 \text{ kHz} \quad \text{Equation 3.8}$$

Only 2% tolerance of the clock is within the range of the PSoC[®] to enable it to talk to the XBee[®] properly. The RX Input used a global bus to connect the external pin. It was set to ROW_0_Input_3 which was connected to pin_2_3. The TX Output also used a global bus to connect the external pin as well. This is set to Row_0_Output_3 which was connected to pin_2_7. The TX Interrupt was set to TXRegEmpty which was best used to maximize the output of the transmitter. The ClockSync parameter was used to control the clock skew and ensure its accurate operation when reading and writing the PSoC[®] block register values. In the research it was set to sync to sysclk. The Command Terminator was where the parameters selected the characters that signalled the end of a command. When it receive data a flag was sent signalling that a complete command has been received. After this flag was set additional characters are not accepted until the cmdReset() function was called. This had been set to 13 which was a carriage return. Figure 3.18 shows the parameter settings.



Name	UART
User Module	UART
Version	5.3
Clock	VC3
RX Input	Row_0_Input_3
TX Output	Row_0_Output_3
TX Interrupt Mode	TXRegEmpty
ClockSync	Sync to SysClk
RxCmdBuffer	Enable
RxBufferSize	16
Command Terminator	13
Param_Delimiter	32
IgnoreCharsBelow	32
Enable_BackSpace	Disable
RX Output	None
RX Clock Out	None
TX Clock Out	None
InvertRX Input	Normal

Figure 3.18 – The UART settings in the API window

3.2.1.6 24-bit Timer

The 24-bit Timer user module provided a down counter with programmable period and capture ability. The clock and enable signals could be selected from any system time base or external source. Once started, the timer operated continuously and reloaded its internal value from the period register upon reaching the terminal count. The output pulses high in the clock cycle following any terminal count. Events can capture the current Timer count value by asserting the edge-sensitive capture input signal. In each clock cycle, the Timer tested the count against the value of the compare register for either a “Less Than” or “Less Than or Equal To” condition. Interrupts may be generated based on terminal count and compare signals.

The 24-bit Timer block diagram is shown in Figure 3.19 and it required three digital block modules to be implemented on the IDE, shown in Figure 3.8 by the purple coloured box, labelled as:

- a. TIMER24_LSB capture
- b. TIMER24_LSB
- c. TIMER24_MSB

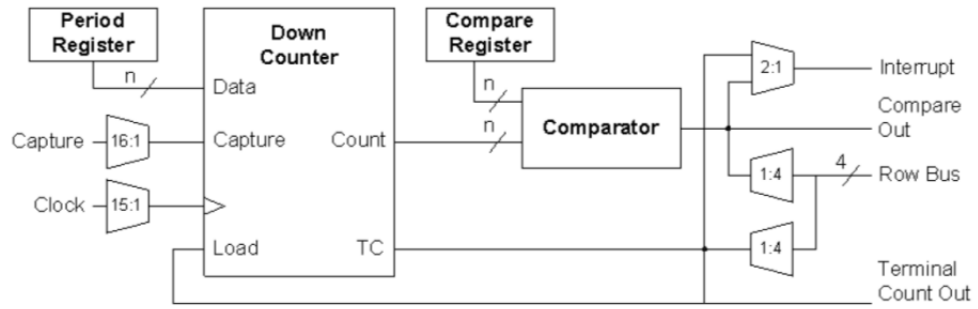


Figure 3.19 – The 24-bit Timer block diagram

Each digital block module contributed 8 bits to the total resolution. The consecutive blocks are linked so their internal carry, terminal count and the compare signals are synchronously chained. This concatenates the 8-bit Count, Period and Compare registers (Data registers DR0, DR1 and DR2, respectively) from block to block to provide the required resolution. The value of the timer period can be calculated using Equation 3.9.

$$\text{Output Period} = \text{Source Clock period} \times (\text{Period Register Value} + 1)$$

Equation 3.9

The output period required for the research was 1 second and the source clock was set at 8 MHz so the period register value, could be calculated using Equation 3.10.

$$\text{Period Register Value} = \text{Output Period Source Clock Period} - 1$$

$$= \frac{1}{8 \times 10^6} - 1 = 7,999$$

Equation 3.10

The clock parameter was selected for VC1 as the VC1 was set to 8 MHz. The capture parameter was set to low as the falling edge of the clock cycle caused the count register to be transferred to the compare register. The period of the timer was set to 7999999. The interrupt type parameter was set to the terminal to count events to trigger the interrupt. The clocksync parameter was set to sync to sysclk. The invert capture was set to normal which determined the sensitivity of the enable input signal to active-high. It would not be using the compare function, so this would not be used.

The API settings are:

- Timer24_EnableInt
- Timer24_Start
- Timer24_Stop

The most important feature was that when programmed the timer interrupt just does not write in the c code file, it also needs to set the assembly code file call: Timer24INT.asm which was the file content timer's interrupt service routine. Under _Timer24_ISR it needed to add a "limp_timercount" to tell the timer where the interrupt would go. Figure 3.20 shows the code that needed to be added.

```
62 | _Timer24_ISR:
63 |
64 | ;@PSoC_UserCode_BODY@ (Do not change this line.)
65 | ;-----
66 | ; Insert your custom assembly code below this banner
67 | ;-----
68 | ; NOTE: interrupt service routines must preserve
69 | ; the values of the A and X CPU registers.
70 | ljmp _timecount
71 | ;-----
72 | ; Insert your custom assembly code above this banner
73 | ;-----
```

Figure 3.20 – Interrupt service routine for Timer24

3.2.2 High-pass Filter

The sEMG signals have a frequency range between 10 Hz to 1 kHz because the PSoC[®] could only configure a low pass filter. An external passive high-pass filter was designed cut the frequency which was around 10 Hz. This research used a passive RC high-pass. The reason for this was to ease the design as only two components are needed; a resistor with a capacitor, see Figure 3.21.

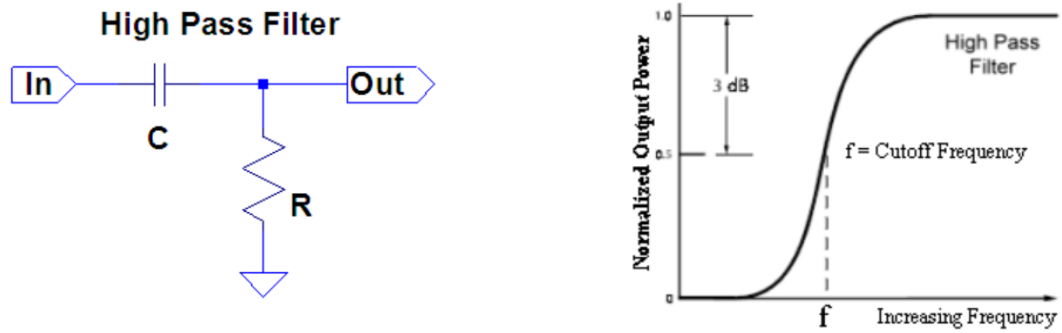


Figure 3.21 – RC Filter Circuit and Frequency Response Diagram

The RC filter was chosen as it was easy to configure and cheaper than an active filter, which would require more components. The value was chosen for the RC passive high filter at 68 kΩ and 0.22 uF, using Equation 3.11, the cut-off frequency was calculated to be at 9.6 Hz, which is very close to the 9.6 Hz required.

$$f_c = \frac{1}{2\pi RC} \quad \text{Equation 3.11}$$

3.2.3 XBee® Transceiver Module

The wireless link chosen was an XBee® RF transceiver module, because this is commonly used in health devices and are easy to configure. These are available from Digi International, USA. XBee® modules are either Series 1 (802.15.4) or XBee® Series 2 (ZB) and are shown in Figure 3.22.

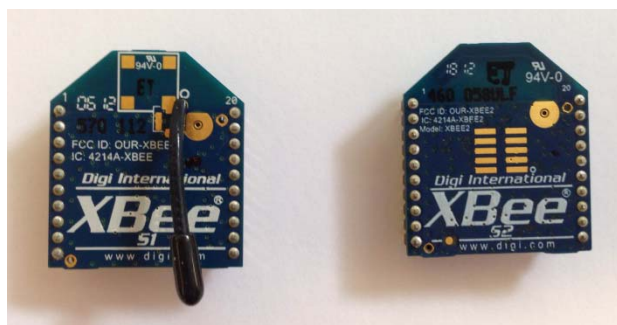


Figure 3.22 – XBee® modules: Series 1 on the left and Series 2 on the right.

Table 3 details the comparisons of a number of technical features extracted from the datasheets for XBee[®] Series 1 and XBee[®] Series 2.

Table 3.1: Product Comparison between XBee[®] Series 1 and XBee[®] Series 2.

<i>Feature</i>	<i>XBee[®] Series 1</i>	<i>XBee[®] Series 2</i>
<i>Indoor/Urban range</i>	up to 100 ft. (30m)	up to 133 ft. (40m)
<i>Outdoor RF line-of-sight range</i>	up to 300 ft. (100m)	up to 400 ft. (120m)
<i>Transmit Power Output</i>	1 mW (0dbm)	2 mW (+3dbm)
<i>RF Data Rate</i>	250 Kbps	250 Kbps
<i>Receiver Sensitivity</i>	-92dbm (1% PER)	-98dbm (1% PER)
<i>Supply Voltage</i>	2.8 - 3.4 V	2.8 - 3.6 V
<i>Transmit Current (typical)</i>	45 mA (@ 3.3 V)	40 mA (@ 3.3 V)
<i>Idle/Receive Current (typical)</i>	50 mA (@ 3.3 V)	40 mA (@ 3.3 V)
<i>Power-down Current</i>	10 uA	1 uA
<i>Frequency</i>	ISM 2.4 GHz	ISM 2.4 GHz
<i>Dimensions</i>	0.0960" x 1.087"	0.0960" x 1.087"
<i>Operating Temperature</i>	-40 to 85 C	-40 to 85 C
<i>Antenna Options</i>	PCB, Integrated Whip, U.FL, RPSMA	PCB, Integrated Whip, U.FL, RPSMA
<i>Network Topologies</i>	Point to point, Star, Mesh (with DigiMesh firmware)	Point to point, Star, Mesh
<i>Number of Channels</i>	16 Direct Sequence Channels	16 Direct Sequence Channels
<i>Filtration Options</i>	PAN ID, Channel & Source/Destination	PAN ID, Channel & Source/Destination

The selection of the XBee[®] transceiver module used for this research was initially determined to be the XBee[®] series 1 module as it was easier to setup for point to point connection. This was used to test the system to be tested and when this was found to be functioning reliably the XBee[®] Series 2 module was used for the research work on the subjects. The difference between the two is that the Series 2 modules are used for mesh networks and can test multiple patterns of movement.

The final development of the WsEMG electrodes used the series 2 transceivers. This would allow for expansion in the number electrode interfaces to be incorporated into a mesh network. By having more than one electrode interface it would be possible to collect EMG signals simultaneously from different sites on a muscle or muscles.

3.2.4 Lithium-ion Polymer (Li-Pol) Battery and Charger

For the WsEMG electrode node to function a battery which is rechargeable, small and light was required. This research used the lithium-ion polymer battery LP-402025-1S-3 as it was suitable for this wireless electrode interface node. The battery chosen required the designing of a suitable battery charger. This was designed as part of the research, see Appendix B for the datasheet.

This lithium-ion polymer battery will need to be charged at regular intervals, so a new charger was required. The battery charger chip used was a LTC4053-4.2 chip is manufactured by Linear Technology, see Appendix C for the datasheet. The reason for choosing this battery charger was because it is a standalone linear charger specially designed for charging the lithium-ion battery. It could be powered directly from a USB port; also it had a thermal regulator to automatically adjust the charge current to limit the battery temperature during charging and in different temperature conditions. The LTC4053-4.2 only needed to use one external resistor to program the charge current; so using Equation 3.12, the resistor value could be calculated.

$$R_{Prog} = \frac{1500 V}{I_{chg}} \quad \text{Equation 3.12}$$

The battery capacity was 155 mAh so when charging the battery it needed the charge current to be very small. For the research the charge current was set to 20 mA. The external resistor value would be 75 kΩ.

3.3 WsEMG Computer Interface Node

The WsEMG computer interface node made the connection between the RF wireless link and the computer. This consists of two components and will be covered in sections:

3.3.1 XBee[®] transceiver module

3.3.2 USB UART chip

The XBee[®] transceiver and USB UART were combined to form the USB dongle. This would be plugged into a USB port of the laptop computer. The sEMG signals would be collected via the USB dongle and would be stored in the laptop for further processing, shown in Figure 3.23.

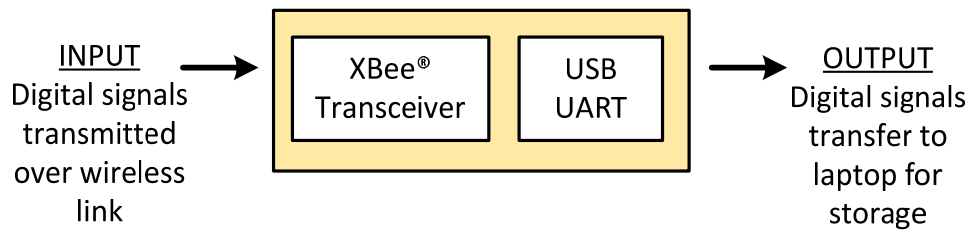


Figure 3.23 – The USB Dongle consisting of the XBee[®] Transceiver and USB UART chip

3.3.1 XBee[®] Transceiver Module

The XBee[®] transceiver attached to the laptop computer interface was the same as described in section 3.2.3. This would be attached to a new USB UART board so that digital signals could be received and transferred to the laptop computer.

3.3.2 USB UART

For the laptop computer to receive the signals from the XBee[®] transceiver a USB UART was included. A FT232R chip was used for the USB to serial UART with an optional clock generator output, and the new FTDIChip-ID™ security dongle manufactured by Future Technology Devices International Ltd (FTDI), UK, see Appendix D for the datasheet. This allowed the use of the WsEMG Computer Interface Node as this would need no external power supply as it would be powered via the USB port of the laptop computer. The following features were the main reasons for choosing the use of the interface chip:

- The entire USB protocol was handled on the chip. No USB specific firmware programming was required.
- The data transfer rates were from 300 baud rate to 3M baud rate.

- The UART interface support would be for 7 or 8 data bits; 1 or 2 stop bits and odd/even/mark/space/no parity.
- The USB 2.0 full speed compatible.

This chapter has presented the methodology used in the design and development of the new WsEMG electrodes used in this research. These consisted of two separate components. The detailed circuitry and new printed circuits boards for the final design of this research will be presented in the next chapter.

Chapter 4

Detail Circuit Diagrams and Printed Circuit Board of Wireless Surface Electrodes

This chapter will show the detailed circuitry and newly manufactured printed circuit boards (PCBs) that make up the components of the WsEMG electrodes system discussed in Chapter 3. These will consist of three main components and are covered in sections:

- 4.1 WsEMG Electrode Interface Node
- 4.2 WsEMG Computer Interface Node
- 4.3 Lithium-ion Polymer Battery Charger

4.1 WsEMG Electrode Interface Node

This node consists of the new main PCB, which has the Cypress PSoC[®] CY8C29466-24PVXA chip plus the necessary components related to it, along with the high-pass filter and the socket for XBee[®] transceiver module plus the three header pins. The header pins are to connect (a) the surface electrodes, (b) the lithium-ion polymer battery and a third (c) which was required only to initially allow the code for the PSoC[®] chip to be downloaded on the chip via the MiniPro1 programmer, which would not be required later when collecting the sEMG signals.

The overall circuit diagram for the main board WsEMG Electrode Interface Node can be found in Appendix E. Figure 4.1 shows the pin layout connections for the PSoC[®] CY8C29466-24PVXA chip along with the external crystal and the RC high pass filter.

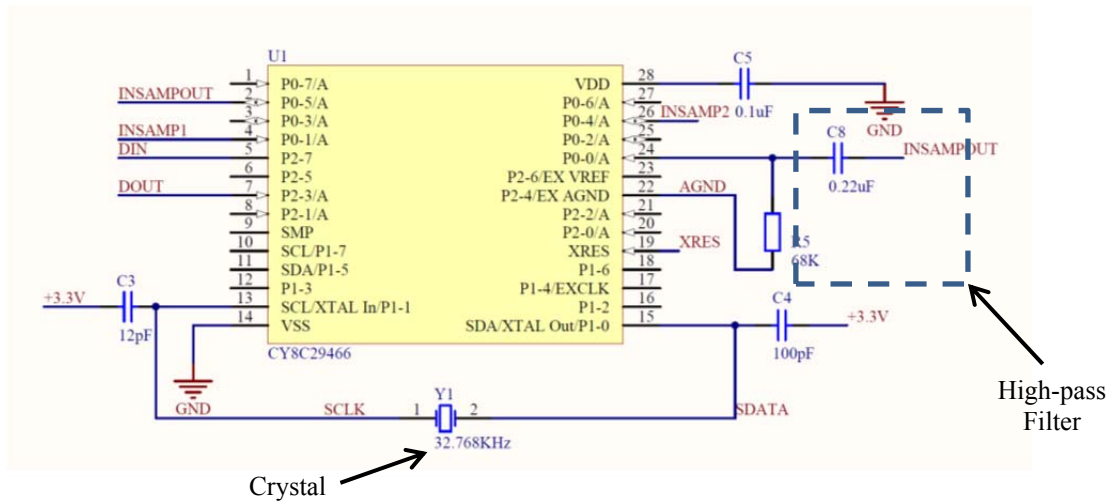


Figure 4.1 – Pin configuration for CY8C29466-24PVXA chip plus components.

The sEMG signals were very small in value with both positive and negative voltages, but the instrumentation amplifier module provided by the PSoC[®] chip could only accept positive voltages as an input. The input gain limit was symmetrical with the analogue ground, so that the input common mode voltage of 0.5V above the Vss (ground) had to have the same input limitation as the input common mode voltage 0.5V below the Vcc (supply). So a DC offset voltage was required for the sEMG signal to fit into this range. This is achieved by using a voltage divider biasing technique and is shown in Figure 4.2. The DC offset was applied to both inputs of the instrumentation amplifier and is 1.65 V ($3.3 \text{ V}/2$) as all the resistors must have equal values.

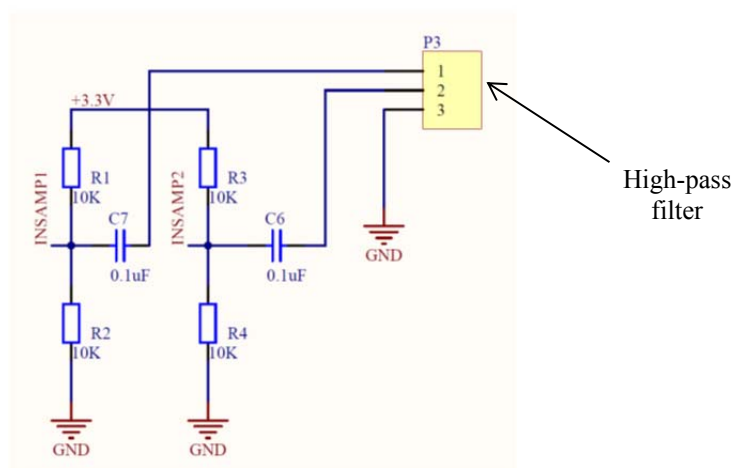


Figure 4.2 – sEMG signal DC offset configuration

The XBee[®] module on the PSoC[®] main board was needed to connect the DOUT pin to the RX pin in PSoC[®] chip; and the DIN pin was connected to TX pin in the PSoC[®] chip. The circuit schematic is shown in Figure 4.3.

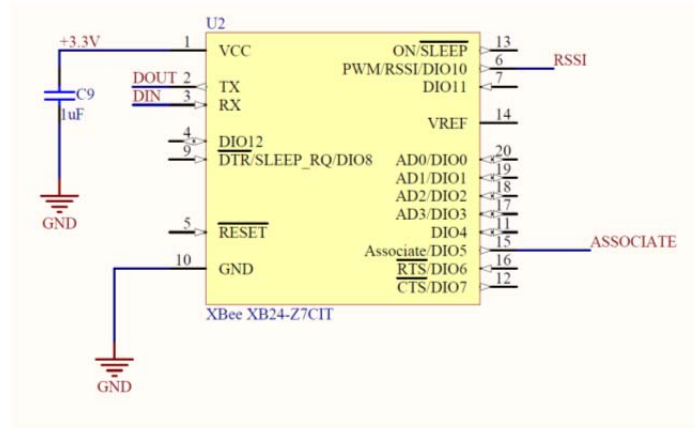


Figure 4.3 – Pin configuration and schematic diagram of XBee[®] module on main board of the WsEMG electrode interface node

The XBee[®] module would only work with a supply voltage of 3.3 V DC but the Lithium-ion polymer battery supplied 3.7 V DC so a DC voltage regulator was needed. The voltage regulator MIC5209-3.3 was a 500 mA low-noise load dropout voltage regulator manufactured by Micrel. A semiconductor was used to supply both the XBee[®] module and the PSoC[®] chip, see Appendix F for this datasheet. The voltage for small loads only required a 10 mV dropout and less than 500 mV at full load. The circuit configuration is shown in Figure 4.4.

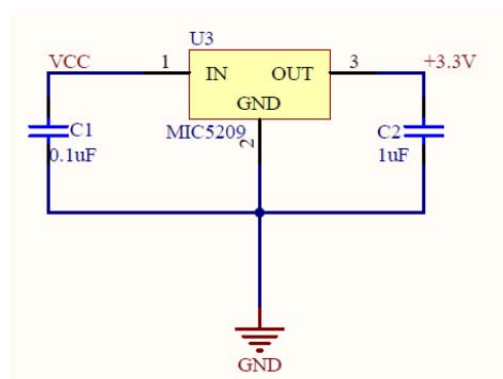


Figure 4.4 – Circuit configuration of MIC5209 voltage regulator for WsEMG electrode interface node

Figure 4.5 shows the components for the main board, the XBee[®] module, the lithium-ion polymer battery, the sEMG electrode leads and the MiniPro1 programmer.

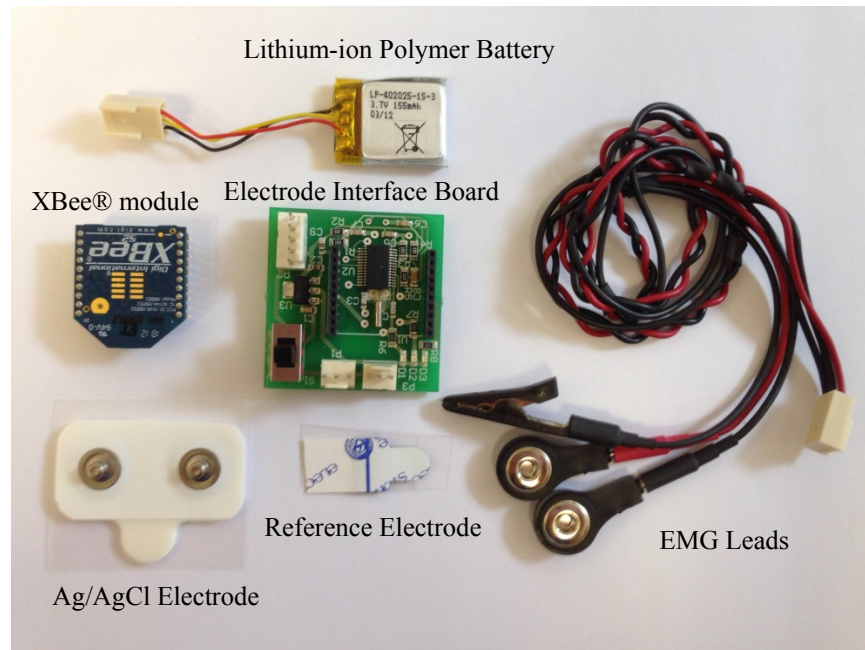


Figure 4.5 – The components that make up WsEMG electrode interface node assembly

Figure 4.6 show pictures of the WsEMG electrode interface node assembled for two different configurations: (a) the top picture shows the initial assembly for the programming of the PSoC[®] chip with the MiniPro1 programmer and (b) the bottom picture shows it when fully assembled for collection of the sEMG signals. The MiniPro1 programmer module allowed for the configuration of files plus the code that had been build and compiled in the PSoC[®] Designer[™] which needed to be downloaded onto the PSoC[®] chip. The code for the WsEMG electrode system is found in Appendix G.

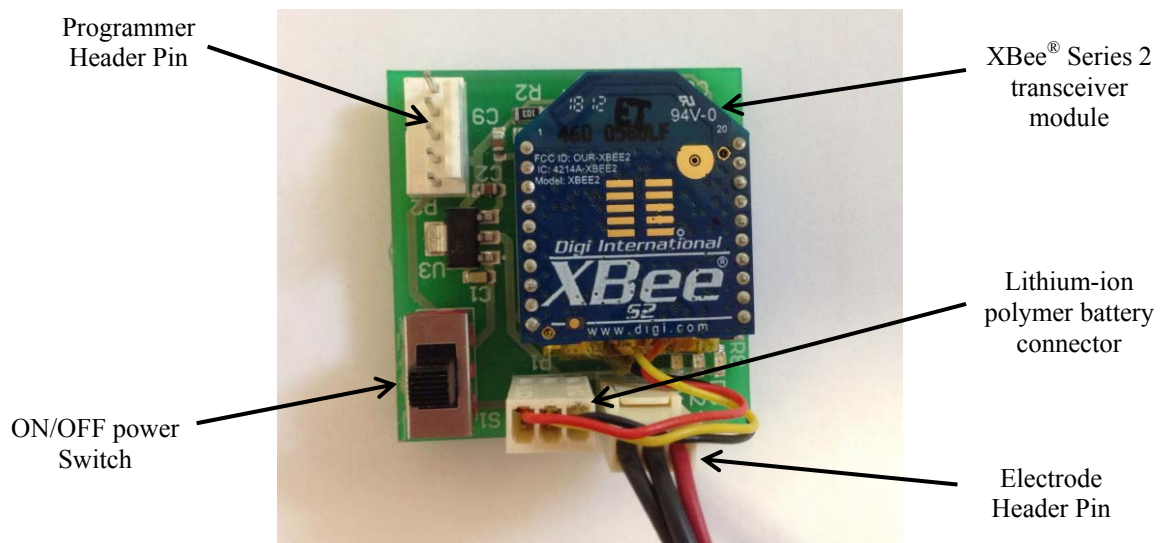
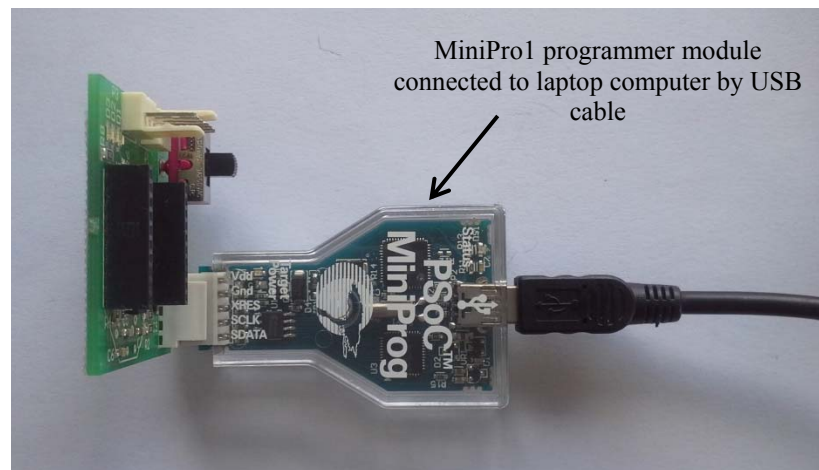


Figure 4.6 – The WsEMG Electrode Interface Node

Overall weight of the board with the XBee® module and battery is 17 grams and the overall dimension is: 42 mm x 41 mm x 20mm.

4.2 WsEMG Computer Interface Node

The overall circuit diagram for the main board WsEMG Computer Interface Node is found in Appendix H. This node consists of a PCB to act as a USB dongle to the laptop computer, which has a socket for the XBee[®] transceiver module and a PCB mounted USB Male Type A connector. The circuit configuration is shown in Figure 4.7.

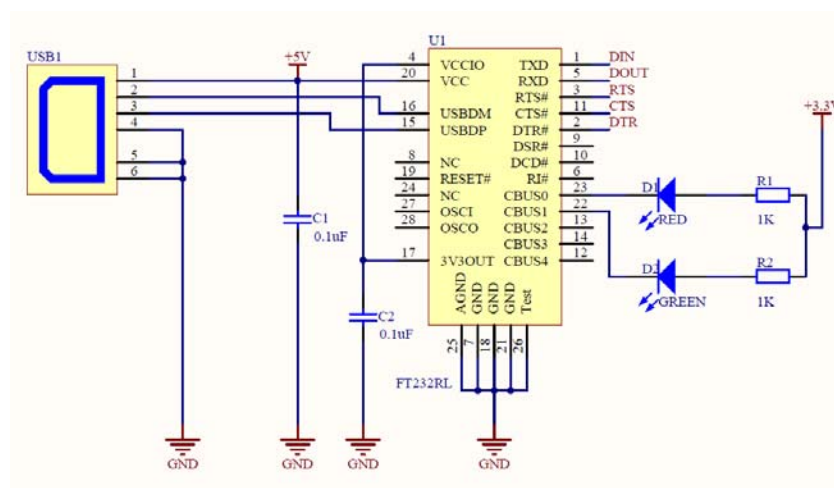


Figure 4.7– Pin configuration and schematic diagram of USB Dongle

The connection between the XBee[®] module and the FT232RL chip required 5 pins to be connected together. These are given in Table 4.1.

Table 4.1 – Shows the Pin Connections for the XBee[®] transceiver module on the USB dongle

<i>FT232 RL Pin No</i>	<i>XBee® Pin No</i>	<i>Name</i>	<i>Description</i>
1	3	DIN	Transmit Asynchronous data output
2	9	DTR	Data terminal ready control output
3	16	RTS	Request to send control output
5	2	DOUT	Receiving asynchronous data input
11	12	CTS	Clear to send control input

The XBee[®] transceiver module circuit diagram and pin configuration was different to the WsEMG electrode node and is shown in Figure 4.8.

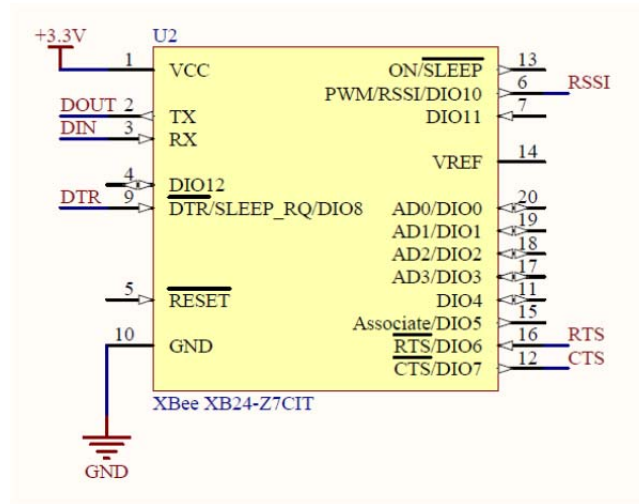


Figure 4.8 – Pin configuration and schematic diagram of XBee[®] module on USB dongle of the WsEMG computer interface node

The supply voltage for the USB dongle PCB was +5 V. The same voltage regulator MIC5209 was used to manage the 3.3 V to the XBee[®] transceiver on this node but with different components, see Figure 4.9.

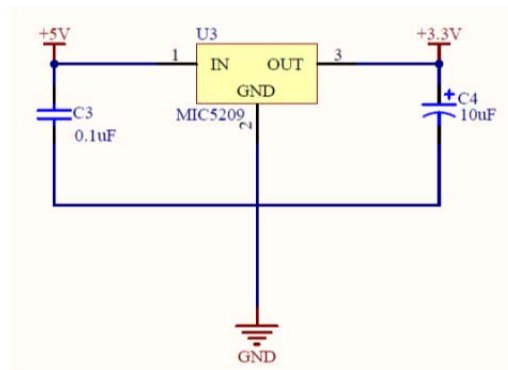


Figure 4.9 – Circuit configuration of MIC5209 voltage regulator for WsEMG computer interface node

Figure 4.10 shows the XBee[®] transceiver module and the new PCB board with the FT232RL chip and voltage before final assembly.

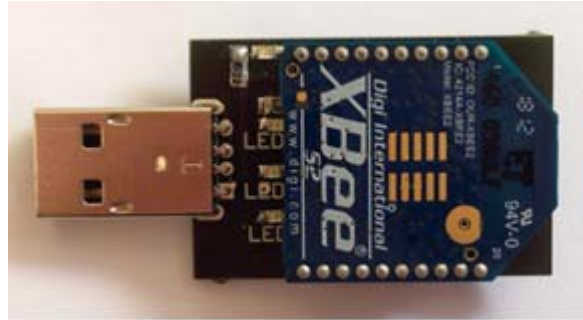


Figure 4.10 – The final PCB with XBee[®] module been attach on.

Figure 4.11 shows the new WsEMG computer interface node attached to a USB port of the laptop computer.

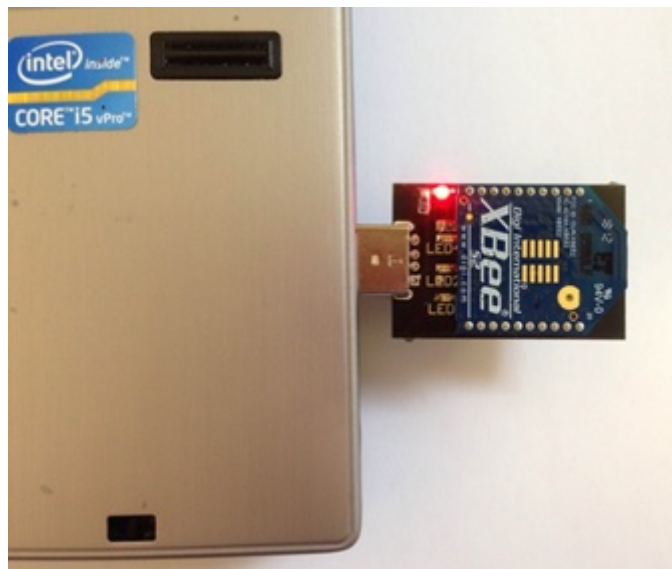


Figure 4.11 – The new WsEMG computer interface node attached to the laptop computer

4.3 Lithium-ion Polymer Battery Charger

The rechargeable lithium-ion polymer battery used for the WSEMG electrode interface node required a new board to be designed and manufactured so the battery could be recharged using the laptop computer USB port. The overall circuit diagram is shown in Appendix I. The circuit schematic for the charging of the LTC4053-4.2 chip used is

shown in Figure 4.12. The three light emitting diodes (LEDs) in the circuit indicated the different states of the charger. At D3 the green LED indicated whether the V_{CC} had been supplied to the circuit or not. Table 4.2 shows LEDs D1 and D2 which indicated the different states whilst the battery was charging.

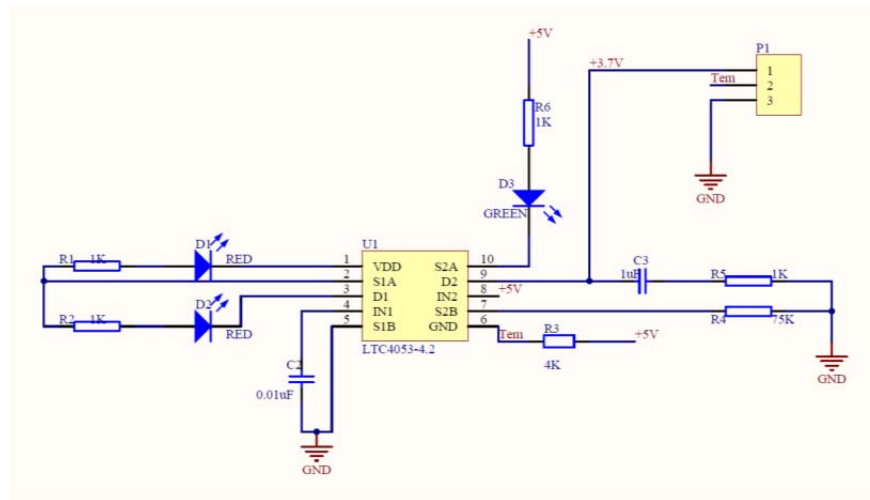


Figure 4.12 – Circuit schematic of battery charger

Table 4.2 – Different states of the Lithium-ion Polymer battery charger

<i>LED D1</i>	<i>LED D2</i>	<i>Description</i>
ON	OFF	Charge cycle has started
ON	ON	Error battery not at the right temperature condition
OFF	OFF	Normal timeout charging has been terminated
OFF	ON	Error battery has a bad cell which cannot be charged

The final layout of the new PCB for the battery charger for the lithium-ion polymer battery is shown in Figure 4.13.

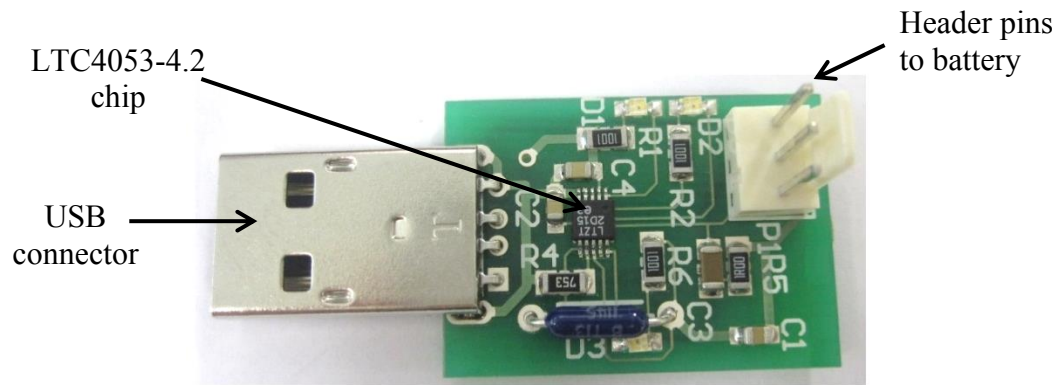


Figure 4.13 – The new Lithium-ion Polymer battery charger

4.4 XBee[®] Wireless Link Configuration

This research used the XBee[®] series 2 transceiver module with a build in antenna version as shown in Figure 4.14.



Figure 4.14 – XBee[®] Series 2 transceiver with build in antenna

XBee[®] transceiver modules came with default factory settings, which can be modified to improve the security of the data being transmitted. To configure the XBee[®] modules the USB dongle described in section 3.3.2 was used to configure both modules separately.

Digi International had customised software to interact with the firmware files found on Digi's wireless products, which had a simple graphical user interface which is called X-CTU. The X-CTU software only needed changes in three different areas, these were:

1. DL (Destination Address Low): was reset/to read the lower 32 bits of the 64 bit destination address. The DH register was set to zero. The DL was less

than 0xFFFF for transmitting using a 16 bit address 0x000000000000FFFF was the broadcast address for the PAN.

2. MY (16-bit Source Address): was set/to read the 16-bit source address for the modem. The MY = 0xFFFF was set to disable the reception of packets with 16-bit addresses. The 64-bit source address was the serial number and was always enabled.
3. BD (Interface Data Rate): was set/to read the serial interface baud rate for communication between the modem serial port and the host. The request for non-standard baud rates with values above 0x80 was used for the terminal window. The BD register had to be read to find the actual baud rate achieved.

Setting for both XBee[®] series 1 and 2 modules are shown below in Table 4.3.

Table 4.3 – Setting made in X-CTU software for XBee[®] Series 1 and 2

Setting	XBee [®] Series 1	XBee [®] Series 2
DL (Destination Address Low)	80	81
MY (16-bit Source Address)	81	80
BD (Interface Data Rate)	7 – 115200	7 – 115200

Figure 4.15 shows the screen shots of the setting made in X-CTU for both XBee[®] modules.

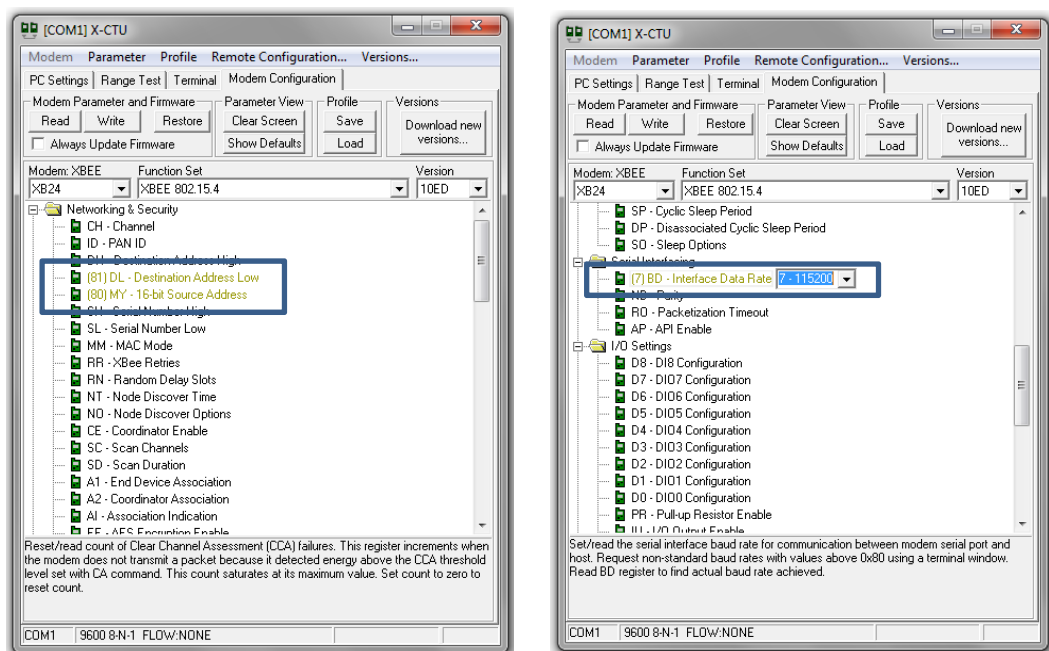


Figure 4.15 – Setting for the XBee[®] Series 2 modules

To test whether the two XBee[®] transceivers were communicating with each, two USB dongles were required with the modules configured. Two X-CTU windows were required to open separately and by typing a statement into one window it would appear in the other window. The other test used to show a certain message was sent by checking the response from the other module to show it had been received. These two tests indicated that the two modules were communicating with each other. This can be seen in Figure 4.16.



Figure 4.16 – The X-CTU window for one XBee[®] module sending a message (blue) with a response from the second XBee[®] module message (red)

4.5 Overall Setup of WsEMG Electrodes

Figure 4.17 shows the electrode interface and computer interface nodes with the surface electrodes connected to a laptop computer ready for the data collection of the sEMG signals from the subject's vastus lateralis muscle.

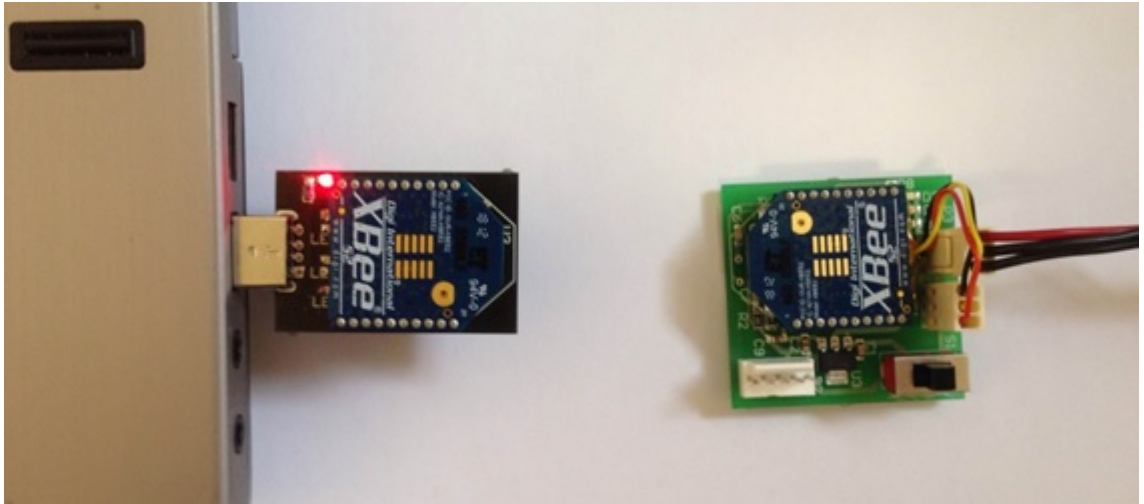


Figure 4.17 – Overall setup of WsEMG system

This chapter has presented the detailed circuitry and the new printed circuits boards for the two nodes that made up the WsEMG system and the battery charger.

The next chapter will present the necessary software that was required to connect the wireless system to the computer in order to collect and store the signals on the designated laptop.

Chapter 5

Graphical User Interface for WsEMG Data Recording

This chapter will discuss the data acquisition of the sEMG signals from the new Wireless Surface (WsEMG) electrode system developed for this research.

This research used LabVIEW software provided by National Instruments to collect the sEMG signals and analysed them. LabVIEW provided a graphical user interface programming code environment, which could be easily configured. There were a large number of functions available for data acquisition, signal conditioning and analysis in this software so it was invaluable for use in this system design.

The WsEMG computer interface node connected to the USB port of the laptop computer FT232RL chip used recognised a serial COM port. This serial COM port needed a software driver interface to connect to the LabVIEW and is called a Virtual Instrument Software Architecture (VISA) and was provided by National instruments. VISA is a standard for configuring, programming, and troubleshooting instrumentation systems comprising GPIB, VXI, PXI, Serial, Ethernet, and/or USB interfaces. Once the driver was installed the LabVIEW could connect to the XBee[®] transceiver module on the USB dongle.

LabVIEW programs are called ‘Virtual Instruments (VI)’ because their appearance and operation imitate physical instruments such as the waveform graph that was needed and used in this research. LabVIEW had a comprehensive set of tools for acquiring, analysing and storing data for the sEMG signals being collected. LabVIEW has two parts; its user interface called the Front Panel with the controls and indicators and the second the Block Diagram where the code is written graphically for the VI to work to analyse the data.

5.1 Main VI

The front panel and the block diagram of the VI for data acquisition for the sEMG system for collecting signals from the vastus lateralis muscle of the subject are shown in Figure 5.1. An enlarged copy of the block diagram is found in Appendix J.

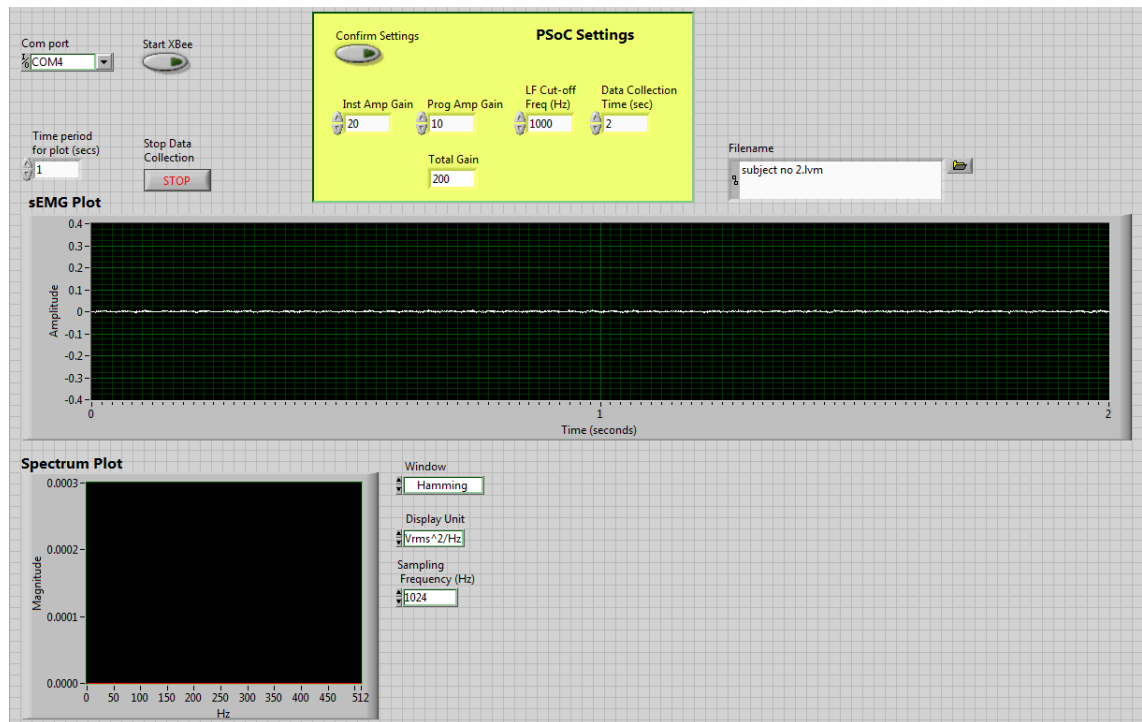


Figure 5.1 – Front Panel (top) and Block Diagram (bottom) of the LabVIEW VI used for data acquisition of sEMG signals.

The VI discussions in this chapter have been split into four sections as follows:

Section 5.2 The Initialisation of the VISA

Section 5.3 The Initial Settings of the PSoC®

Section 5.4 The Plotting of the sEMG signal

Section 5.5 The Power Spectrum of the sEMG signal

5.2 Initialisation of the VISA

To allow the XBee[®] modules on the dongle and main boards of the system to start sending data, the VISA configuration serial port function node had to be set. The two settings required were:

1. The setting of the *com port* from the USB dongle for the communications. This was done on the front panel of the VI.
2. The *baud rate* for XBee[®] module to communicate with the PSoC[®] chip.

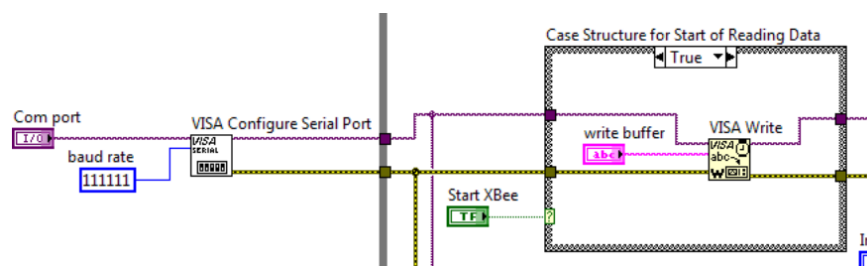


Figure 5.2 – Section of the VI block diagram for configuring the VISA function node of the main LabVIEW VI

Once the *com port* and *baud rate* had been set, the XBee[®] start control button on the front panel could be pressed to start the XBee[®] modules to communicate with the laptop computer.

5.3 Initial Settings of the PSoC®

The front panel instrumentation allowed different setting to be chosen for the parameters of the PSoC® chip. This is shown on Figure 5.3, these are:

1. The Instrumentation Amplifier gain
2. The Programmable Gain Amplifier
3. The Low-pass filter cut-off frequency
4. The Time setting of the PSoC® for collecting the data

These setting were made on the front panel of the VI and once the Confirm Settings control had been pressed each of the above setting were sent in sequence to the PSoC® chip to be set before the data was transferred to the laptop computer.

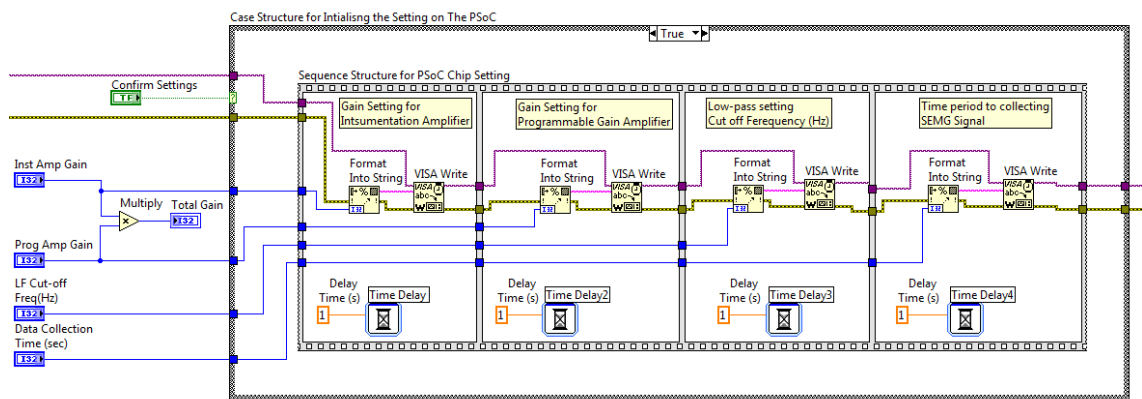


Figure 5.3 – Section of the VI block diagram for configuring the amplifiers, low-pass filter and time period on PSoC®

5.4 Plotting of the sEMG signal

Once the PSoC® transmitted the data via the XBee® transceiver modules it did so continuously. To display this on the front panel of the main VI the data had to be split into segments. The technique used to achieve this is shown in Figure 5.4.

The data from the VISA read function node on the block diagram was fed into the while loop to split the data stream into values which could then be plotted. This was done by identifying the spaces which separated the data into individual values ready for plotting.

This chapter has presented the LabVIEW VI software that was developed for the data collection of sEMG signals for the new WsEMG electrode system developed for this research. The protocol for the collection of the sEMG signals plus a set of results taken from the subject's vastus lateralis muscle using the new WsEMG electrodes will be presented in the next chapter.

Chapter 6

Testing Procedures and Results

This chapter will describe the testing protocol that was approved by the Auckland University of Technology (AUT) Ethics Committee. These are detailed in Appendix K. A single set of results was collected using the newly designed WsEMG electrodes with the newly VI developed using the LabVIEW software.

6.1 Testing Protocol

The following steps were taken in collecting the sEMG signals from the subjects who had volunteered to be part of this research.

6.1.1 Procedure

When potential participants made contact with the researcher they were screened using inclusion and exclusion criteria, this is detail in Appendix K. If the subject was deemed to be suitable to participate in the study, they received a verbal explanation of what would be involved. Prior to assessment, procedures were explained to the participant and time was given for each participant to have any remaining questions answered before their individual written consent was obtained.

6.1.2 Maximal Strength Test

Participants were expected to perform a five-minute generalised warm up that would include riding an exer-cycle at a self-selected pace and performing a range of motion exercises for the lower limbs.

After the general warm-up was completed, the participants were seated in the upright chair of the HUMAC®/NORM™ Testing and Rehabilitation System (Computer Sports Medicine, Inc) with the selected knee bent to 80 degrees and attached to a load cell that measured the voluntary isometric force of the quadriceps.

The upper body and upper thigh of the subject was securely strapped to the chair and the leg was also strapped to the load cell at mid-shin level, as shown in Figure 6.1. The subject was then asked to perform a specific warm-up and was familiarised with a series of four sets of short (5 seconds) sub-maximal isometric knee extensions. The intensity of the contractions was gradually increased against the resistance of the load cell and within the subject's own limits.

A one-minute rest followed each set of warm-up contractions. The subject was then rested for three minutes before the maximal voluntary isometric force (MVIF) of the quadriceps was measured. Three MVIF's were measured and recorded for a five-second period. There was then a two-minute rest period between each MVIF test and the highest MVIF was then selected for analysis.

Standardised verbal encouragement was given throughout the test from the force-to-failure point.

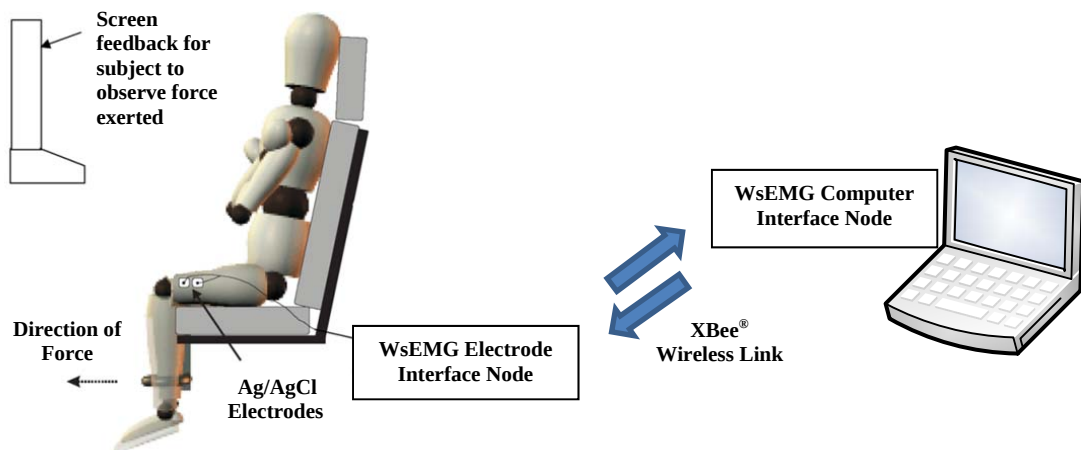


Figure 6.1 – Schematic diagram showing the equipment setup for data acquisition of sEMG signals.

6.1.3 Isometric Contraction Knee Extension Test

The subjects were rested for a further period of 20 minutes following the maximal strength test, before the subjects were again asked to maintain a sub-maximal contraction at 50% MVIF for a ten-second period. Subjects were also instructed prior to and during the tests to endure the contractions required using standardised verbal encouragement.

6.1.4 Electromyography (EMG) Measures:

Muscle activity was recorded using the new WsEMG electrode system designed for this research. Following appropriate skin preparation (the skin was shaved, then gently abraded and cleaned with alcohol), the surface Ag/AgCl surface electrodes were then placed on the skin surface overlying the vastus lateralis muscle of the thigh using standardised procedures.

6.2 Results

The new WsEMG was tested on five healthy volunteers with no previous history of knee or severe musculoskeletal injuries (five males, aged between 18-35 years) participated in this study.

Figure 6.2 shows placement of both the Ag/AgCl electrodes on the vastus lateralis muscle of the subjects and the reference electrode as per recommendations published by the Surface Electromyography for Non-invasive Assessment of Muscle[35].



Figure 6.2 – Placement of Electrodes on Subjects Leg

Figure 6.3 shows the Electrode Interface Node attached the surface electrodes on the subjects prior to testing.

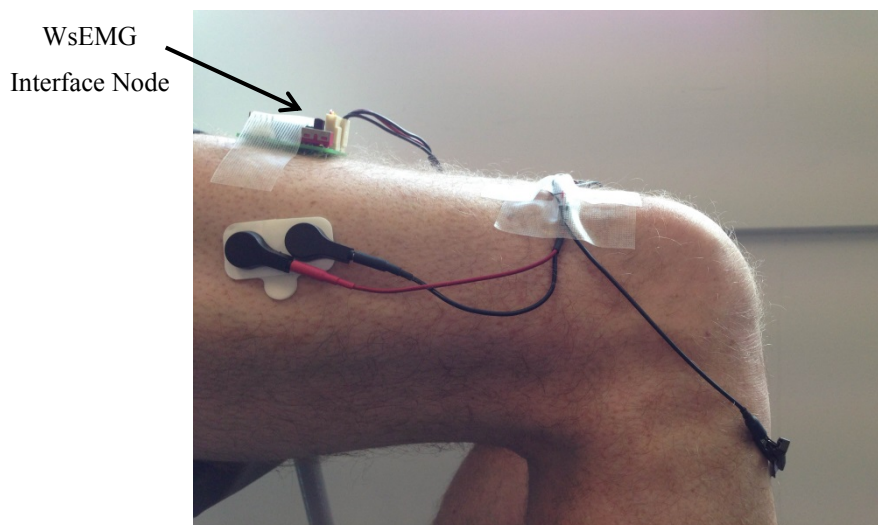


Figure 6.3 – Placement of Electrodes on Subjects Leg

Figure 6.4 shows a one second period of sEMG signal collected from Subject No. 2 vastus lateralis muscle performing 50% Maximum Voluntary Isometric Force (MVIF) contraction as per the testing protocol approved by the AUT Ethics Committee.

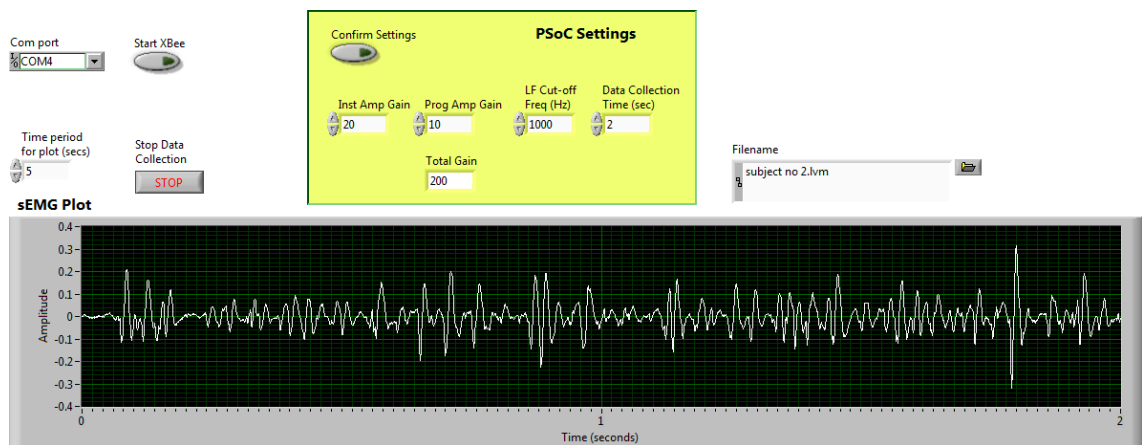


Figure 6.4 – sEMG signal at 50% MVIF from Subject No.2

Figure 6.5 shows the corresponding Power Spectrum plot for the sEMG signal shown in Figure 6.4

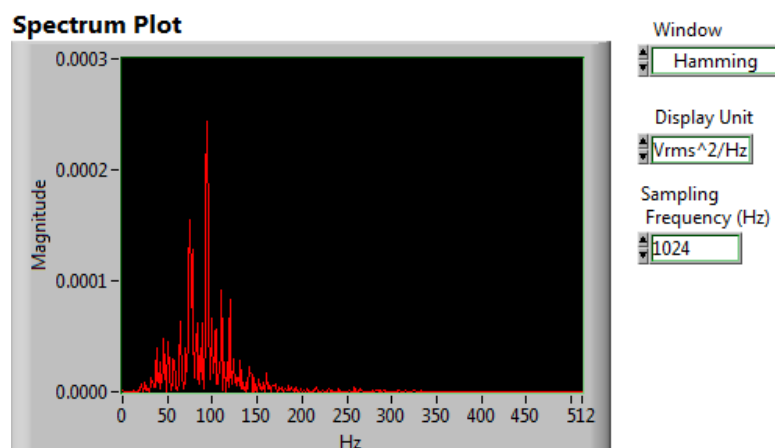


Figure 6.5 – Power Spectrum for sEMG shown in Figure 6.4

The outcome of this research showed that the new developed WsEMG electrode system using the PSoC[®] chip using XBee[®] series 2 transceivers modules with a new VI developed using LabVIEW code produce acceptable results in terms of the data collection of sEMG signals.

Chapter 7

Conclusion and Future Work

This research was designed to show the potential in building a new light and compact wireless electrode system for data acquisition of sEMG signals. The prototype system consisted of two parts (a) the electrode interface node and (b) the computer interface node. The XBee[®] series 2 transceiver modules were used for the wireless link between the two nodes.

The data acquisition and storage of the data on a laptop computer was achieved by developing a new virtual instrument using LabVIEW software. By using the PSoC[®] chip with LabVIEW it was possible to reconfigure a number of settings such as the overall gain and low-pass cut off frequency by using software without having to physically change the hardware components which made the system more flexible and easier to use.

The overall system acquired sEMG signals sampled at a sampling frequency of 1048 Hz with an overall gain of 200. The signals collected using human subjects after gaining the AUT Ethics Committee's approval gave acceptable results compared to wired electrodes in terms of signal quality. This research has shown that using the new WsEMG electrodes would enhance the ability of the clinician to collect sEMG signals without the need to put patients or subjects under unrealistic test conditions.

Future work is required to solve a number of issues, these are:

1. The present configuration of the XBee[®] transceiver modules had been configured using a point to point network. As the modules were series 2 which supports mesh networking, future work is required to understand how this would be implemented using more than one node on a muscle site or testing different muscles at the same time.

2. The prototype device at present requires both nodes to be handled with care. It requires some skill to place one on the subject's skin and the other on the USB interface. So new enclosures will be required to be designed. This will require greater consideration of the PCB layout and connectors.
3. The rechargeable battery needs to be removed from the electrode interface node when it needs to be recharged using an external battery charger. It would be more suitable to have the charger become part of the interface node board. This would then need a new circuit and PCB board to manage the battery charger circuit. This could still be on the same board as the PSoC[®] chip with the XBee[®] modules. This would still require this board to be light and compact.

Appendix A:

Datasheet for PSoC[®] CY8C29466-24PVXA Chip

Glossary (continued)

- | | |
|--------------------------------|---|
| base | 1. A systematic deviation of a value from its reference value.
2. The amount by which the average of all values departs from its reference value. |
| block | 1. The physical, mechanical, magnetic, or other (redundant) applied or data device to establish a reference level to a system.
2. A functional unit that may be configured to perform one or several functions, such as a digital PASC block or an analog PASC block. |
| buffer | 1. A device used to store a single data item, such as an analogizer.
2. A functional unit that may be configured to perform one or several functions, such as a digital PASC block or an analog PASC block. |
| buffer | 1. A storage area that is used to compensate for a speed difference, when transferring data from one device to another. Usually refers to an area reserved for I/O operations. This buffer data is read, or it is written into, from a device.
2. A portion of memory set aside to store data, often before it is sent to an external device or as it is received from an external device. |
| bus | 1. An organized connection for the output of information of a system.
2. A network of connections for data, bundling lines together in a bus matrix to ease the route with similar routing. |
| clock | 1. A set of digital performing a common function and carrying similar data. Typically represented using vector notation.
2. One or more conditions that serve as a common criterion for a group of related devices. |
| comparator | The device that compares a digital signal with a fixed frequency and duty cycle. A clock is sometimes used to synchronize digital logic blocks. |
| complex | An electronic circuit that produces an output voltage or current whenever the input levels simultaneously satisfy predetermined amplitude requirements. |
| computer | A program that translates a high-level language, such as C, into machine language. |
| condition | 1. A program that translates a high-level language, such as C, into machine language.
2. A logic device, the register space within the XC324, in the CPLD X register, is set to |
| converter | An application in which the frequency is controlled by a programmable clock. Typically a programmable clock is less sensitive to ambient temperature than other control components. |
| crystal oscillator | A calculation used to select even input data communications, typically performed using a linear feedback shift register. Similar calculations may be used for a variety of other purposes such as data compression. |
| cyclic redundancy check (CRC) | A bit-directional set of logic used by a computer to convey information from memory location to the control processing unit and vice versa. More generally, a set of signals used to convey data between digital functions. |
| data bus | A hardware and software system that allows to analyze the operation of the system under development. A hardware and software system that allows to analyze the operation of the system under development. A hardware and software system that allows to analyze the operation of the system under development. |
| debugger | A period of time when the developer is deep through the timeline one step at a time, at break points, and |
| delay block | A period of time when either of two or more signals are in their deliverable or a transition. |
| digital blocks | The built logic blocks that can be used or reuse; time, actual number; serial transfer; CLIC generator; parallel transfer; parallel transfer; CLIC generator. |
| digital signal processor (DSP) | 1. A digital signal processor that is used to process digital signals.
2. A digital signal processor that is used to process digital signals. |

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Glossary (continued)

- | | |
|---------------------------------|---|
| data cycle | The relationship of a clock period T_{clk} to its live time, expressed as a percent. |
| divider | Deductive logic or reduction of the functions of one system with a different system; e.g., the second system's divider divides the first system's divider by two. |
| emulator | An active high signal that is shown in the PSoC device. It causes all operations of the CPU peripherals to stop and return to their initial state. |
| external reset
(RES) | An externally programmable and enableable, non-volatile hardware bit provides you the programmability and control of PSoCs. This bit is system-enabling. Non-volatile means that the data is stored when power is lost. |
| flash | An electrical storage element that stores data that may be programmed at one time and the available amount of data can vary to be protected. |
| frequency | The number of cycles or events per unit of time, for a periodic function. |
| gain | The ratio of current, voltage, or power to input current, voltage, or power, respectively. Gain is usually positive. |
| I ² C | A two-wire serial interface based on Philips Semiconductor's two-wire (SMBus) communication. It is used for low-speed peripheral in a embedded system. The original system was created in the early 1980s as a battery-powered protocol for interconnecting sensors and actuators in a distributed environment. Today, I ² C is used in many more industrial applications, such as data and control bus among ICs, video equipment and disk drive systems. This bus operates up to 100 kHz based on standard mode and up to 500 kHz based on fast mode versions. |
| ICE | The on-chip emulator that allows you to test the program in a hardware environment, while viewing the debugging device activity in a software environment (PSoC Designer). |
| input/output (I/O) | A device that introduces data into or extracts data from a system. |
| interrupt | A suspension of a process, such as the execution of a computer program, caused by an event external to that process, and performed at a time when it would be desired that the process can be resumed. |
| interrupt service routine (ISR) | A block of code that interrupt code executes whenever a CPU receives a hardware interrupt. Many times, the ISR contains code that performs some action on the interrupt source. |
| jitter | With a microcontroller, timing of the device is the point in the program when a normal program execution will meet an interrupt handling. The jitter is the variation of the time taken for an interrupt to occur on several data streams. |
| load | The load is the sum of the capacitance of the pins of the device, which is connected to other devices, successively loaded. The amplitude of a continuous cycle, the frequency or phase of a continuous cycle. |
| low-voltage detect (LVD) | A circuit that senses VDD and provides an interrupt to the system when VDD falls below a selected threshold level. |
| MDC | A 16-bit Harvard architecture microprocessor. The microprocessor coordinates all activity made a PSoC by interfacing to the flash, SRAM, and register space. |
| master device | A device that controls the timing of data exchange between two devices. Or when devices are cascaded in a daisy chain, the master device initiates the transfer of data. The master device also generates the clock signal between the cascade devices. |

CY8C29466, CY8C29666

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Glossary (continued)

- | | |
|------------------------------|---|
| microcontroller | An integrated circuit chip that is designed primarily for control systems and products. In addition to a CPU, a microcontroller typically includes memory (flash, ROM, and SRAM), and I/O circuitry. This reason for its use is to permit the user to design a system that is more compact and efficient. The microcontroller is normally not used for general-purpose computers and is a microprocessor. |
| mixed signal IC | This reference to a circuit containing both analog and digital techniques and components. |
| modem | A device that imposes a signal on a carrier. |
| modulator | 1. A technique that allows a signal and any other desired information carried by the signal.
2. The random variations of one or more characteristics of any entity such as voltage, current, or data. |
| oscillator | A circuit that may be crystal controlled and is used to generate a clock frequency. |
| parity | A technique for detecting transmission data. Typically, a binary digit is added to the data to make the sum of all the data bits an even number. |
| phase-locked loop (PLL) | An electronic circuit that connects an oscillator to a feedback system to maintain a constant phase angle relative to a reference signal. |
| processor | The main computer equipment, the relation between the signal on each of the outputs of the processor device and the physical components in the printed circuit board (PCB) package. It provides also input/output as a link between microcontroller and PCB design (both being computer generated) files. It may also involve pin numbers. |
| port | A group of pins, usually eight. |
| power on reset (POR) | A circuit that forces the processor to reset when the voltage is below a pre-set level. This is on output of a voltage divider. |
| PS/2® | Cypress Semiconductor's PS/2C™ is a registered trademark, and Programmable System on Chip™ is a trademark of Cypress. |
| PS/2C Design™ | This software for Cypress' Programmable System on Chip technology. |
| pulse width modulation (PWM) | An output in the form of duty cycle which varies as a function of the signal value. |
| RAM | An acronym for random access memory. A data storage device from which data can be read out and new data can be written in. |
| register | A storage device with a specific capacity, such as a bit or byte. |
| resistor | A means of limiting a system's capacity to draw below a known state. See hardware and software used. |
| ROM | An acronym for read only memory. A data storage device from which data can be read out, but new data cannot be written in. |
| serial | 1. Pertaining to the sequence of events across one wire or other.
2. Pertaining to the sequence of a consecutive occurrence of two or more related activities in a single device or system. |
| setting time | The time it takes for an output signal or value to stabilize after the input has changed from one value to another. |

Glossary (continued)

- | | |
|-----------------|--|
| shift register | A memory storage device that sequentially shifts a word either left or right to a stream of serial data. |
| slave device | A device that follows a master device to transfer data, such as a peripheral device. When two or more devices are associated with, the slave device is the one that allows another device to control the timing of data transfer between the associated devices and an external interface. The controlling device is called the master device. |
| SRAM | An acronym for static random access memory. A memory device where you can store and retrieve data at any rate of speed. The semiconductor uses transistors, after a value is loaded into an SRAM cell, it remains unchanged until it is explicitly altered or until power is removed from the device. |
| SRIO | An acronym for serial rapid IO. The SRIO holds code that is used to boot the device, calculate checksums, and manage I/O operations. The functions of the SRIO may be accelerated in some user code, operating on a flash. |
| stop bit | A signal following a character or block that prepares the receiving device to receive the next character or block. |
| synchronous | 1. A signal whose state is not acknowledged or acted upon till the next active edge of a clock signal.
2. A system whose operation is synchronized to a clock signal. |
| 3-tuple | A data structure used to adopt three values, 0, 1, and 2 (3-tuple pointers). The tuple does not give any information about the order of the values, but it is guaranteed to be constructed with the same values, allowing another object to have the same set. |
| UART | A UART or universal asynchronous receiver-transmitter transmits between parallel bits of data and serial bits. |
| user modules | Pre-built or vendor-developed firmware modules in a system that take care of managing and configuring the lower level analog and digital I/Fs of blocks. User modules also provide high level API Application programming interfaces for the peripheral function. |
| user space | The third 64 space of the register map. The registers in this bank are more likely to be modified during normal operation. The registers in this bank are likely to be modified only during initialization phase of the program. |
| V _{DD} | A name for a power net internally "voltage source". The most positive power supply signal. Usually 1V or 1.3 V. |
| V _{DD} | A name for a power net internally "voltage source". The most negative power supply signal. |
| watchdog timer | A timer that must be serviced periodically. If it is not serviced, the CPU results after a specified period of time. |

Appendix B:

Datasheet for Lithium-ion Polymer Battery LP- 402025-1S-3

Specification of

Li-polymer Rechargeable Battery

Model No.: LP-402025-1S-3

Reported by: 陈宇 Date: Jan.02.2012
Checked by: _____ Date: Jan.02.2012
Approved by: _____ Date: Jan.02.2012

- rated capacity.
- 4.3.11 Open Circuit Voltage: 3.6V ~ 4.1V as of shipment.
- 4.4 Mechanical Performance
- 4.4.1 Vibration Test: 95% (min) of Rated Capacity, No Leakage
After standard charge (Section 4.3.1), the battery is vibrated with an amplitude of 0.8mm (1.6mm total maximum excursion) for 60 minutes in three mutually perpendicular directions. The vibration is performed between 10Hz and 55Hz at a rate of 1Hz per minute.
After the completion of the vibration, the capacity shall be measured at a discharge current of 2.75V
- 4.5 Environmental Performance: of 2.75V
- 4.5.1 Thermal Shock Test: No Leakage, No Fire, No Explosion
The battery is stored at 75°C±5°C for 48 hours, moved to a temperature of -20°C±5°C within 5 minutes and stored for 6 hours after standard charge (Section 4.3.1).
- 4.6 Safety Performance
- 4.6.1 Short Circuit Test: No Fire, No Explosion
After standard charge (Section 4.3.1), the battery shall be subjected to a short-circuit condition with a wire of resistance less than50mΩfor 1 hour
- 4.6.2 Overcharge Test: (with a PCM) No Fire, No Explosion
After standard charge (Section 4.3.1), the battery shall be charged at 1C/12V For 2.5 hrs.
- 4.6.3 Thermal Exposure Test: No Fire, No Explosion
After standard charge (Section 4.3.1), the battery is placed in an oven and is heated up at a rate of 5°C until the temperature reaches 130°C. The oven shall be maintained at 130°C for 60 minutes.

5. **Delivery Condition:** about 90%-charged.
6. **Lithium Ion Polymer Battery Handling Guideline**
- 6.1 In case of contacting the materials from a damaged or returned cell or battery:
Eye contact: Washing immediately with plenty of water and soap for at least 15 minutes.
Skin Contact: Washing immediately with water and soap. Inhalation of Vented Gas: Remove to fresh air. Get medical attention. Ingestion: Get medical attention immediately.
- 6.2 Keep away batteries from children.
- 6.3 The cells/batteries are requested to be stored within a proper temperature range specified in the specification.
- 6.4 Do not place batteries in a manner that allow a terminals to short circuit.
- 6.5 Do not place batteries near heating sources, nor exposed to direct sunlight for long periods. Elevated temperatures can result in reduced battery service life.
- 6.6 Charging Battery
Use only approved chargers and procedures. Improperly charging a cell or battery may cause

1. **Scope**
This specification describes the definition, technical requirement, testing method, warning and caution of the Lithium ion polymer rechargeable battery. The specification only applies to DUBILERS Li-ion battery.

2. **Product Model**
Battery type: Rechargeable Lithium-ion Polymer Battery
Battery Model: LP-402025-1S-3

3. **Ratings**
- 3.1. Nominal Capacity(at 0.2C): 155mAh (min), 165mAh (typical)
3.2. Nominal Voltage: 3.7V (average voltage at 0.2C discharge)
3.3. Charging Voltage: 4.20 ±0.05V
3.4. Mins. Charging Current: 155mA
3.5. Charging Method: constant current constant voltage
Standard Charge: 78mA (constant current) charge to 4.20V, then 4.2V (constant voltage) for 3.5hr or 3mA(0.02C) cut off
155mA(constant current) charge to 4.20V, then 4.2V (constant voltage) for 3.0hr or 3mA(0.02C) cut off
3.6. Mins. Continuous Discharge Current: 3.5A
3.7. Discharge Cutoff Voltage: 2.75V
3.8. Battery Dimensions (Refer to the attached drawing)
- Thickness: 3.8±0.3
Width: 20±1
Length: 26±1
3.9 Battery Weight: 440±2g
3.10 Operating Temperature Discharge: -20°C ~ -60°C
Charging: 0°C ~ +45°C
Storage in a 50% charged state Temperature range: Duration Typ. Capacity recovery

- the cell or battery to flame or damage.
- Change the battery using the "CC/CV" or constant current, constant voltage method.
- Do not charge the battery with a current or voltage higher than the specified maximum value in this specification. The absolute maximum charging voltage is 4.25V per cell.
- Prohibit reverse charging of the battery. The battery must be connected correctly.
- 6.7 Discharging Battery
Discharge battery at the max current specified in this specification. If you plan to discharge battery at a higher current than the max current, please consult us.
- Do not over-discharge the battery. Over-discharging can damage the performance of the battery. It should be noted that the cell/battery would be at an over-discharge state by its self-discharge characteristics in case the cell is not used for long time. In order to prevent over-discharging, the cell/battery shall be charged periodically to maintain between 3.7V and 4.1V.
- 6.8 Operation Temperature
The battery shall be operated (stored, charged and discharged) in the temperature specified in 6.9.
- 6.9 Cell/Battery Protection Circuit Module (PCM)
The cell/battery must be equipped with a PCM that protects the cell/battery from overcharging, over-discharging and over-current.
- 6.10 Battery Short Circuit
Do not short-circuit a battery. A short circuit can result in over-heating of the terminals and provide an ignition source. More than a momentary short circuit will generally reduce the cell or battery service life and can lead to ignition of surrounding materials or materials in contact with the battery. Do not attempt to short circuit the battery. The battery has a high temperature in the cell and at the terminals. Physical contact to high temperature can cause skin burns. In addition, extended short-circuit may cause the cell or battery to flame.
- 6.11 Prohibit reversing cell polarity within a battery assembly.
- 6.12 The cell edge of the heat seal zone is electrically conductive. Avoid the edge cross battery terminals, PCB, or conductive surfaces.
- 6.13 Do not bend, fold or fill the battery or part of the battery. It may cause the battery be damaged and result in the battery swelling, leaking, explosion or ignition
- 6.14 Do not use the battery in the following conditions:
6.15 Do not bend or fold the sealing edge. And do not tear off the sealing film.
- 6.16 Battery Pack Design
The battery housing should have sufficient mechanical strength.
No sharp edge components shall be inside the battery housing. The sharp edge may destroy the cell packaging.
No cell movement is allowed in the battery housing.
The ultrasonic head shall not directly or indirectly pressed the cell if you need to enclose the battery housing by ultrasonic method. Please consult us for designing the ultrasonic head and designing a right battery housing.
- 6.17 Battery Assembly
We recommend ultrasonic welding or spot welding to connect battery with PCM, please pay attention to the following:

- 20°C ~ -80°C 10 days 50%(expected)
-20°C ~ -60°C 1month 75%(expected)
-20°C ~ +45°C 3months 70%(expected)
-20°C ~ +25°C 1year 80%(expected)

4. Battery Performance

- 4.1. Visual Inspection
There shall be no such defects as remarkable scratches, cracks, leakage or deformations.
- 4.2. Test Condition
Test new cells within one month after shipment from our factory and the cells shall not be cycled over five times before the tests.
- All the tests in this specification shall be conducted in an ambient temperature of 25°C
- 4.2.1 Capacity Retention: 85% (minimum) of Rated Capacity
Capacity Recovery: 90% (minimum) of Rated Capacity
The capacity retention shall be measured at a discharge current of 0.2C and a cut-off voltage of 2.75V after standard charge (Section 4.3.1) and being stored for 28 days at 25°C±5°C. Then, the capacity recovery shall be measured at a discharge current of 0.2C and a cut-off voltage of 2.75V after standard charge (Section 4.3.1).
- 4.2.2 Measuring humidity of 25% to 85%, unless otherwise specified.
- 4.2.2.1 The dimension measurement shall be implemented by instruments with equal or more precision of 0.01mm.
- 4.2.2.2 Standard class specified in the national standard or more sensitive class having inner impedance more than 10kΩV.
- 4.2.2.3 Impedance shall be measured by a sinusoidal alternating current method (1MHz/LCR meter).
- 4.2.2.4 The current measurement shall be implemented by instrument with equal to more precision scale of±0.1% and the constant voltage precision should be implemented within±0.5%, and the timing precision should be not below ±0.1%.
- 4.2.2.5 The temperature measurement shall be implemented by instrument with equal or more precision seat of ±0.5°C.
- 4.3 Electrical Characteristics
- 4.3.1 Standard Charge
The cell shall be charged at a constant current of0.5C to 4.2V and then at constant voltage of 4.2V for 3.5 hours or 0.02C cut off.
- 4.3.2 Rated Capacity
The capacity shall be measured at a discharge current of 0.2C and a cut-off voltage of 2.75V after the standard charge (Section 4.3.1)
- 4.3.3 High Rate Discharge Capacity (1C): 85% (minimum) of Rated Capacity
The capacity shall be measured at a discharge current of 1C and a cut-off voltage

- Use a solder with temperature controlled and ESD.
- Soldering temperature should not exceed 300°C.
- Soldering time should not be longer than 3s.
- Soldering times should not exceed 5 times.
- Keep battery tab cold down before next time soldering.
- Do not directly heat cell body. It may cause the battery be damaged by heat above 90°C
- 6.18 Battery Disassembly
Never disassemble a battery.
- Should a battery unintentionally be crushed, thus releasing its contents, rubber gloves must be used to handle all battery components. Avoid inhalation of any vapors that may be emitted.
- 6.19 Do not mixed Batteries and Types. Avoid to use old and new cells or cells of different sizes, different chemistry or types in the same battery assembly.
- 6.20 Other Warnings
Do not immerse or submerge the battery in fire, water or other liquid.
Do not put the battery into microwave, washing machine or drying machine.
- 6.21 Others
Distributor shall make no liability for problems that occur when the above specifications are not followed.
7. **Remarks**
If any matter with this specification arises, it shall be revised by mutual agreements.

8. Drawing

of 2.75V after the standard charge (Section 4.3.1).

4.3.4 Low Temperature Discharge Capacity(0°C): 80% (minimum) of Rated Capacity
The capacity shall be measured at a discharge current of 0.2C in an ambient temperature of 0°C±2°C and a cut-off voltage of 2.75V after the standard charge (Section 4.3.1)

4.3.5 Low Temperature Discharge Capacity(-10°C): 70% (minimum) of Rated Capacity
The capacity shall be measured at a discharge current of 0.2C in an ambient temperature of -10°C±2°C and a cut-off voltage of 2.75V after the standard charge (Section 4.3.1)

4.3.6 High Temperature Discharge Capacity(60°C): 100% (minimum) of Rated Capacity
The capacity shall be measured at a discharge current of 0.2C in an ambient temperature of 60°C±2°C and a cut-off voltage of 2.75V after the standard charge (Section 4.3.1)

4.3.7 Storage Characteristics (25°C)

Capacity Retention: 85% (minimum) of Rated Capacity
Capacity Recovery: 90% (minimum) of Rated Capacity
The capacity retention shall be measured at a discharge current of 0.2C and a cut-off voltage of 2.75V after standard charge (Section 4.3.1) and being stored for 28 days at 25°C±5°C. Then, the capacity recovery shall be measured at a discharge current of 0.2C and a cut-off voltage of 2.75V after standard charge (Section 4.3.1).

4.3.8 Storage Characteristics (45°C)

Capacity Retention: 60% (minimum) of Rated Capacity
Capacity Recovery: 70% (minimum) of Rated Capacity
The capacity retention shall be measured at a discharge current of 0.2C and a cut-off voltage of 2.75V after standard charge (Section 4.3.1) and being stored for 28 days at 45°C±5°C. Then, the capacity recovery shall be measured at a discharge current of 0.10C and a cut-off voltage of 2.75V after standard charge (Section 4.3.1)

4.3.9 Internal Impedance: 25 5mΩ (Type) ; 42mΩ(max)

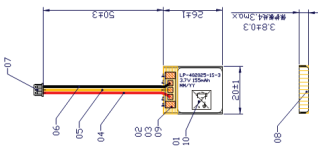
The internal impedance shall be measured at a sine wave alternative current process of 1kHz after the standard charge.

4.3.10 Cycle Life:

The cycle life shall be conducted as the following procedures :

- Step 1: charge the cell with the standard charge (as of section 4.3.1);
Step 2: discharge the cell at 0.5C to 2.5V;
Step 3: repeat Step 1 and Step 2 for 500 times.
The capacity after 300 cycles is expected to be equal to or more than 80% of the rated capacity. The capacity after 500 cycles is expected to be equal to or more than 60% of the

序号	零件名称	规格
01	PCB/Cell	402025P
02	PCB	3000A 2.5V 4444444444444444
03	PCB/ATC	ATC 04142
04	PCB/Red Wire(+)	UL1064H28
05	PCB/Yellow Wire(-)	UL1064H28
06	PCB/Black Wire(-)	UL1064H28
07	PCB/connector	FS101-3P 4444444444444444
08	PCB/Insulating Top	4444444444444444 Orange
09	PCB/Insulating Top	4444444444444444 Orange
10	PCB/Label	00-7977 4444444444444444



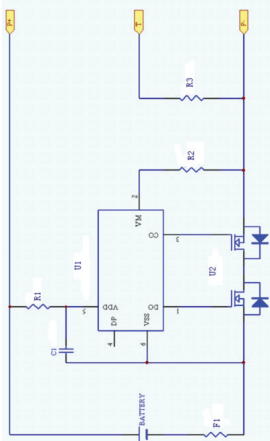
Data sheet for protect circuit board

- Over-charge-Current:
4-A.13 Short Protection Voltage: 0.55V (min) 0.8 V (Typ) 1.0V (max)
4-A.14 Output Delay of 230(Min) 300 μs(Typ) 500μs(max)
Short Protection:
4-A.15 Supply Current (active status): 4.0μA (Typ) 8.0μA (max)
4-A.16 Supply Current (Standby): 1.2μA (Typ) 2.00μA (max)
4-A.17 PCM Resistance : 35mΩ(min) 50mΩ(Typ) 60mΩ(max)

5. Part List

Part Number	Part Name	Qty	Remark
Ricoh RS402N04KD or Equivalent	Control IC	1	U1
SM5S205 or S1S205 or SM5S207or Equivalent	MOSFET	1	U2
330c2(0603)	Resistor	1	R1
1kΩ(0603)	Resistor	1	R2
10kΩ(7(0603)	NTC	1	R3
SM12080(1812)	PTC	1	F1
0.1μf(0603)	Capacitor	1	C1

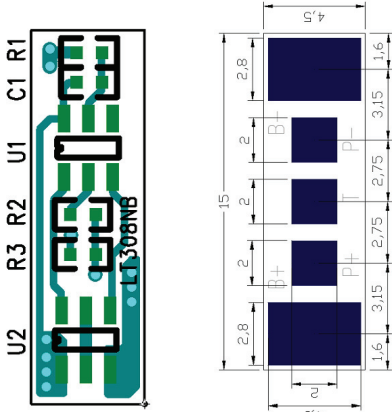
6. PCM Circuit Diagram (RS402N04KD or Equivalent)



1. Type and Model
2. Type: Protection Module for Li Ion/Li-Polymer Battery Pack
3.1 Absolute Maximum Ratings (for Ricoh RS402N05KD)
3.2 Supply Voltage: -0.3V to 12 V
3.3 Operating Temperature: -40°C to 85°C
3.4 Storage Temperature: -55°C to 125°C
4. Electrical Characteristics (for Ricoh RS402N04KD(T=-25°C)
The followings is referring to the specs of RS402N04KD of Ricoh (for details,
see RS402N04KD). These specs are guaranteed by design not by production tests.

- 4-A.1 Input Voltage: 1.5V (min) 5.0V(max)
4-A.2 Overcharge Detection : 4.175V (min) 4.20V(Typ) 4.225V(max)
4-A.3 Output Delay of Overcharge: 0.7s (min) 1.0s(Typ.) 1.3s (max)
4-A.4 Overcharge Release : 3.85V (min) 3.90V(Typ) 3.93V(max)
4-A.4 Over-discharge Detection : 2.438V (min) 2.500V(Typ) 2.562V(max)
4-A.5 Output Delay of Over-discharge: 14ms (min) 20ms(Typ) 26ms(max)
4-A.6 Over-discharge Release : 2.925V (min) 3.000V(Typ) 3.075V(max)
4-A.7 Over Discharge-Current Detection: 0.185V (min) 0.20V(Typ) 0.225V(max)
4-A.8 Overcharge-Current Detection : 0.17V (min) 0.20V(Typ) 0.23V(max)
4-A.9 Over Discharge-Current Value: 3.0A(min) 4.0A(Typ) 7.0A (max)
4-A.10 Over-charge-Current Value: 3.0A(min) 4.0A(Typ) 7.0A (max)
4-A.11 Output Delay of Over-Discharge-Current: 8ms (min) 12ms(Typ) 16ms (max)
4-A.12 Output Delay of 5ms (min) 8ms(Typ) 11ms (max)

7. PCB layout(RS402N04KD OR Equivalent)PCN0308NB



Appendix C:

Datasheet for Battery Charger LTC4053-4.2 Chip

Appendix D:

Datasheet for FT232R Chip



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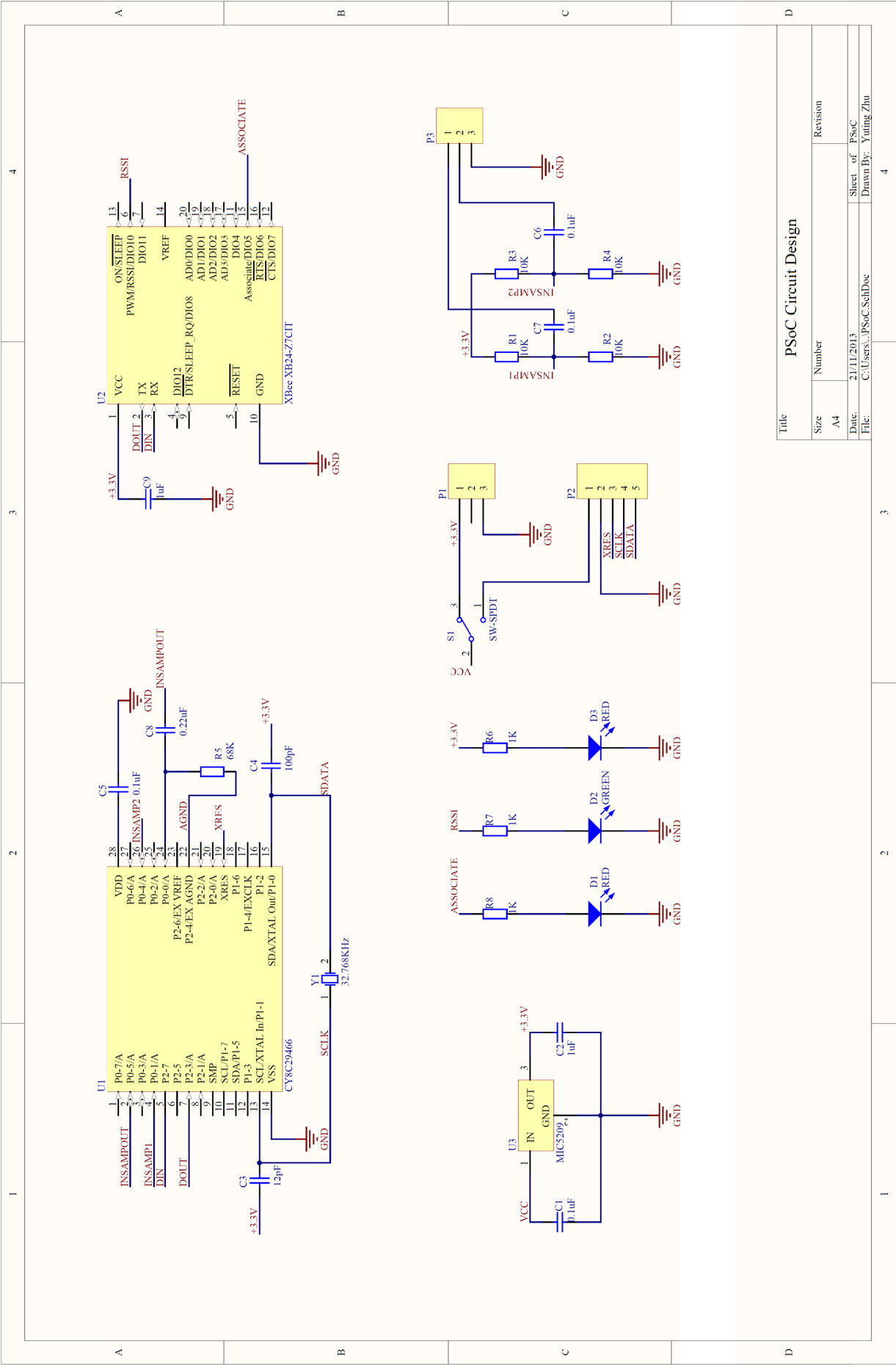
Appendix C Revision History

Document Title:	USB UART IC FT232RL
Document Reference No.:	FT_000053
Clearance No.:	FTID# 310
Product Page:	http://www.ftdichip.com/Products.htm
Document Feedback:	Send Feedback

Version 0.1B	Initial Datasheet Created	August 2005
Version 0.1C	Revised Pin-related datasheet	October 2005
Version 0.1D	Added USB Powered Configuration	December 2005
Version 1.0.0	Added USB Powered Configuration	December 2005
Version 1.0.1	Manufacturer ID added to default EPROM configuration (Burr-Brown added)	January 2006
Version 1.0.2	LFN-32 Pad layout and solder paste diagrams added	January 2006
Version 1.0.3	Reformatted, updated package info, added notes for 3.3V operation	June 2007
Version 2.0.0	Part numbers, TID-backed UART and CBUS characteristics for +1.1V	
Version 2.0.1	Corrected the input switching threshold and input hysteresis values for VCCIO-5V	
Version 2.0.2	Corrected pin-out number in table 3.2 for CND pin 11	
Version 2.0.3	Added package pin numbers	
Version 2.0.4	Added package pin numbers	
Version 2.0.5	Added package pin numbers	
Version 2.0.6	Added package pin numbers	
Version 2.0.7	Added package pin numbers	
Version 2.0.8	Added package pin numbers	
Version 2.0.9	Added package pin numbers	
Version 2.1.0	Added package pin numbers	

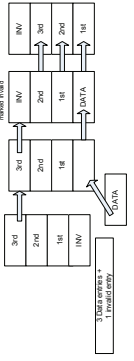
Appendix E:

**Circuit Diagram for the WsEMG Electrode
Interface Node**



Appendix F:

Datasheet for XBee[®] Series 2 Module



User Bindings
These entries can be created and maintained by the application if needed. The following information can be used to modify the user bindings. See the command descriptions for formatting details.

Table 4-63. User Bindings

Command	Name	Description
B	Source Binding	Source address of the remote node (hex)
B	Source Binding	Source address of the remote node (hex)
B	Source Binding	Source address of the remote node (hex)

Network Addressing
The ZigBee specification is a broadcast technology that only has a limited number of addresses. The network address is a 16-bit address that is used to identify a node in the network. The network address is a 16-bit address that is used to identify a node in the network. The network address is a 16-bit address that is used to identify a node in the network.

Endpoint Addressing
The ZigBee specification, either ASCII, and HexStream application have reserved some endpoints for different uses. These endpoints are not available for user applications. The endpoints are not available for user applications. The endpoints are not available for user applications.

4.2.3. Xbee Series 2 Endpoint Table
The Xbee Series 2 module maintains a table of supported endpoints. If an endpoint will be used as the source endpoint or a data transmission, the endpoint must first be defined in the endpoint table.

Table 4-64. Endpoint Table

Endpoint	Name	Description
1	Endpoint 1	Endpoint 1
2	Endpoint 2	Endpoint 2
3	Endpoint 3	Endpoint 3

Command Endpoint
The command endpoint is used to send or reply to various commands. The command endpoint is used to send or reply to various commands. The command endpoint is used to send or reply to various commands.

Data Endpoint
This endpoint is used to send serial data to other Xbee Series 2 modules. It must always exist in the application.

1x Explicit Endpoint
This entry is used as needed to define the source endpoint that must be defined for a data transmission. The source endpoint is used to define the source endpoint that must be defined for a data transmission.

User Endpoints
These endpoints are controlled entirely by the application. These endpoints may be added, removed, or viewed in the RF module using the following commands: AT+ENDPOINT, AT+ENDPOINT, AT+ENDPOINT.

Table 4-65. ZigBee Data Transmission Addressing Table

Command	Name	Description
E1	Endpoint 1	Endpoint 1
E2	Endpoint 2	Endpoint 2
E3	Endpoint 3	Endpoint 3

4.3. Advanced Network Features

Network Mapping
Network mapping is the process to identify all devices on a PAN. There are currently two ways to map the network. The first way is to use the AT+MAP command. The second way is to use the AT+MAP command.

Node Discovery (ND) Command
The ND command is used to discover the nodes on the network. The ND command is used to discover the nodes on the network. The ND command is used to discover the nodes on the network.

API Child Joined Indicator
The API child joined indicator is used to indicate when a child node has joined the network. The API child joined indicator is used to indicate when a child node has joined the network. The API child joined indicator is used to indicate when a child node has joined the network.

Configurable A/D and Digital Lines
The following table lists the pin functions supported on the modules.

Table 4-66. Configurable A/D and Digital Lines

Pin Name	Module Pin Number	Configuration Command
AD0	10	AD0=0
AD1	11	AD1=0
AD2	12	AD2=0
AD3	13	AD3=0
AD4	14	AD4=0
AD5	15	AD5=0
AD6	16	AD6=0
AD7	17	AD7=0
AD8	18	AD8=0
AD9	19	AD9=0
AD10	20	AD10=0

Setting the configuration command that corresponds to a particular pin will configure the pin. Parameters for the pin configuration commands typically include the following:

Table 4-67. Pin Configuration Parameters

Pin Name	Module Pin Number	Configuration Command
AD0	10	AD0=0
AD1	11	AD1=0
AD2	12	AD2=0
AD3	13	AD3=0
AD4	14	AD4=0
AD5	15	AD5=0
AD6	16	AD6=0
AD7	17	AD7=0
AD8	18	AD8=0
AD9	19	AD9=0
AD10	20	AD10=0

Sampling A/D and Digital Input Lines
The AT+PINUP command can be used to enable the input of all enabled A/D and digital input lines. The AT+PINUP command can be used to enable the input of all enabled A/D and digital input lines.

Table 4-68. Sampling A/D and Digital Input Lines

Pin Name	Module Pin Number	Configuration Command
AD0	10	AD0=0
AD1	11	AD1=0
AD2	12	AD2=0
AD3	13	AD3=0
AD4	14	AD4=0
AD5	15	AD5=0
AD6	16	AD6=0
AD7	17	AD7=0
AD8	18	AD8=0
AD9	19	AD9=0
AD10	20	AD10=0

The AT+PINUP command can be used to enable the input of all enabled A/D and digital input lines. The AT+PINUP command can be used to enable the input of all enabled A/D and digital input lines. The AT+PINUP command can be used to enable the input of all enabled A/D and digital input lines.

Table 4-69. Sampling A/D and Digital Input Lines

Pin Name	Module Pin Number	Configuration Command
AD0	10	AD0=0
AD1	11	AD1=0
AD2	12	AD2=0
AD3	13	AD3=0
AD4	14	AD4=0
AD5	15	AD5=0
AD6	16	AD6=0
AD7	17	AD7=0
AD8	18	AD8=0
AD9	19	AD9=0
AD10	20	AD10=0

5. Xbee Series 2 Command Reference Tables
Special Command Table

Table 5-1. Special Command Table

Command	Name	Description	Pin Type	Parameter Range	Default
W	Wake Up	Wake up the module from sleep mode.	DIG	0	0
W	Wake Up	Wake up the module from sleep mode.	DIG	0	0
W	Wake Up	Wake up the module from sleep mode.	DIG	0	0

Non-type not supported the command: C - Coordinate, R - Route, E - End Device

Table 5-2. Xbee Series 2 Command Reference Tables

Command	Name	Description	Pin Type	Parameter Range	Default
AT	AT Command	AT Command	DIG	0	0
AT	AT Command	AT Command	DIG	0	0
AT	AT Command	AT Command	DIG	0	0

Table 2-1. Xbee Series 1 Command Reference Tables

Command	Name	Description	Pin Type	Parameter Range	Default
SC	Serial Command	Serial Command	DIG	0	0
SC	Serial Command	Serial Command	DIG	0	0
SC	Serial Command	Serial Command	DIG	0	0

Non-type not supported the command: C - Coordinate, R - Route, E - End Device

Table 2-2. Xbee Series 1 Command Reference Tables

Command	Name	Description	Pin Type	Parameter Range	Default
AT	AT Command	AT Command	DIG	0	0
AT	AT Command	AT Command	DIG	0	0
AT	AT Command	AT Command	DIG	0	0

Table 2-3. Xbee Series 1 Command Reference Tables

Command	Name	Description	Pin Type	Parameter Range	Default
AT	AT Command	AT Command	DIG	0	0
AT	AT Command	AT Command	DIG	0	0
AT	AT Command	AT Command	DIG	0	0

Non-type not supported the command: C - Coordinate, R - Route, E - End Device

Table 2-4. Xbee Series 1 Command Reference Tables

Command	Name	Description	Pin Type	Parameter Range	Default
AT	AT Command	AT Command	DIG	0	0
AT	AT Command	AT Command	DIG	0	0
AT	AT Command	AT Command	DIG	0	0

Appendix G:

**PSoC[®] Designer[™] Code for the WsEMG
Electrode System**

PSoC C code

```
//
// Wireless Electrode Code for PSoC
//
// Written by Yuting Zhu
//
// 2013
//

//-----
// C main line
//-----

#include <m8c.h>          // part specific constants and macros
#include "PSoCAPI.h"      // PSoC API definitions for all User Modules
#include "stdlib.h"
#include "delay.h"
#include "string.h"
#pragma interrupt_handler timecount
char *command;
int ADC_Output;
int *status;
int *status1;
int run;
int INSAMPIN;
int INSAMPOUT1;
int INSAMPOUT2;
int x=0;
char start[] = "start";
char stop[] = "stop";
char F1000[] = "F1000";
char F900[] = "F900";
char F800[] = "F800";
char F700[] = "F700";
char F600[] = "F600";
char F500[] = "F500";
char PGA0_5[]="PGA0_5";
char PGA1[]="PGA1";
char PGA2[]="PGA2";
char PGA4[]="PGA4";
char PGA8[]="PGA8";
char PGA16[]="PGA16";
char PGA24[]="PGA24";
char PGA48[]="PGA48";
char INSAMP0_5[]="INSAMP0_5";
char INSAMP1[]="INSAMP1";
char INSAMP2_5[]="INSAMP2_5";
char INSAMP5[]="INSAMP5";
char INSAMP10[]="INSAMP10";
char INSAMP20[]="INSAMP20";
char INSAMP30[]="INSAMP30";
char INSAMP60[]="INSAMP60";
char INSAMP93[]="INSAMP93";
char S10[]="S10";
char S20[]="S20";
char S30[]="S30";
```

```

char S60[]="S60";
char S90[]="S90";
char S120[]="S120";
char S180[]="S180";
char S240[]="S240";
char S300[]="S300";
int time;

void startpro(void)
{
    INSAMP_Start(INSAMP_HIGHPOWER);
    PGA_Start(PGA_HIGHPOWER);
    LPF2_Start(LPF2_HIGHPOWER);
    DelSig_Start(DelSig_HIGHPOWER);
    DelSig_StartAD();
    Delay10msTimes(10);
    Timer24_Start();
    Timer24_EnableInt();
}

void stoppro(void)
{
    INSAMP_Stop();
    PGA_Stop();
    LPF2_Stop();
    DelSig_Stop();
    DelSig_StopAD();
    Timer24_Stop();
}

void initial(void)
{
    run=0;
    LPF2_SetC1(5);
    LPF2_SetC2(5);
    LPF2_SetC3(12);
    LPF2_SetC4(26);
    LPF2_SetCA(LPF2_FEEDBACK_32);
    LPF2_SetCB(LPF2_FEEDBACK_32);
    PGA_SetGain(PGA_G1_00);
    INSAMP_Set2StageGain(INSAMP_INGAIN_1, INSAMP_OUTGAIN_1_00);
    time=10;
    stoppro();
}

void main(void)
{
    UART_CmdReset();
    UART_IntCnt1(UART_ENABLE_RX_INT);
    UART_Start(UART_PARITY_NONE);

    // Uncomment this line to enable Global Interrupts
    M8C_EnableGInt;

    // Insert your main routine code here.
    initial();
    while(1)
    {

```

```

if(UART_bCmdCheck())                // Wait for command
{
    if(command = UART_szGetParam()) // When the command is sent to uC
    {
        if(!strcmp(command,start))
        {
            startpro();
            run=1;
        }
        else if(!strcmp(command,stop)) // command:
        {
            stoppro();
            run=0;
        }
        else if(!strcmp(command,F1000))
        {
            LPF2_SetC1(5);
            LPF2_SetC2(5);
            LPF2_SetC3(12);
            LPF2_SetC4(26);
        }
        else if(!strcmp(command,F900))
        {
            LPF2_SetC1(4);
            LPF2_SetC2(4);
            LPF2_SetC3(13);
            LPF2_SetC4(23);
        }
        else if(!strcmp(command,F800))
        {
            LPF2_SetC1(4);
            LPF2_SetC2(4);
            LPF2_SetC3(11);
            LPF2_SetC4(25);
        }
        else if(!strcmp(command,F700))
        {
            LPF2_SetC1(4);
            LPF2_SetC2(4);
            LPF2_SetC3(9);
            LPF2_SetC4(28);
        }
        else if(!strcmp(command,F600))
        {
            LPF2_SetC1(2);
            LPF2_SetC2(2);
            LPF2_SetC3(14);
            LPF2_SetC4(16);
        }
        else if(!strcmp(command,F500))
        {
            LPF2_SetC1(3);
            LPF2_SetC2(3);
            LPF2_SetC3(7);
            LPF2_SetC4(29);
        }
        else if(!strcmp(command,PGA0_5))
        {

```

```

        PGA_SetGain(PGA_G0_50);
    }
    else if(!strcmp(command,PGA1))
    {
        PGA_SetGain(PGA_G1_00);
    }
    else if(!strcmp(command,PGA2))
    {
        PGA_SetGain(PGA_G2_00);
    }
    else if(!strcmp(command,PGA4))
    {
        PGA_SetGain(PGA_G4_00);
    }
    else if(!strcmp(command,PGA8))
    {
        PGA_SetGain(PGA_G8_00);
    }
    else if(!strcmp(command,PGA16))
    {
        PGA_SetGain(PGA_G16_0);
    }
    else if(!strcmp(command,PGA24))
    {
        PGA_SetGain(PGA_G24_0);
    }
    else if(!strcmp(command,PGA48))
    {
        PGA_SetGain(PGA_G48_0);
    }
    else if(!strcmp(command,INSAMP0_5))
    {
        INSAMP_Set2StageGain(INSAMP_INGAIN_1,
            INSAMP_OUTGAIN_0_50);
    }
    else if(!strcmp(command,INSAMP1))
    {
        INSAMP_Set2StageGain(INSAMP_INGAIN_1,
            INSAMP_OUTGAIN_1_00);
    }
    else if(!strcmp(command,INSAMP2_5))
    {
        INSAMP_Set2StageGain(INSAMP_INGAIN_2,
            INSAMP_OUTGAIN_1_25);
    }else if(!strcmp(command,INSAMP5))
    {
        INSAMP_Set2StageGain(INSAMP_INGAIN_4,
            INSAMP_OUTGAIN_1_25);
    }else if(!strcmp(command,INSAMP10))
    {
        INSAMP_Set2StageGain(INSAMP_INGAIN_8,
            INSAMP_OUTGAIN_1_25);
    }else if(!strcmp(command,INSAMP20))
    {
        INSAMP_Set2StageGain(INSAMP_INGAIN_16,
            INSAMP_OUTGAIN_1_25);
    }else if(!strcmp(command,INSAMP30))
    {

```

```

        INSAMP_Set2StageGain(INSAMP_INGAIN_24,
                              INSAMP_OUTGAIN_1_25);
    }
    else if(!strcmp(command,INSAMP60))
    {
        INSAMP_Set2StageGain(INSAMP_INGAIN_48,
                              INSAMP_OUTGAIN_1_25);
    }
    else if(!strcmp(command,INSAMP93))
    {
        INSAMP_Set2StageGain(INSAMP_INGAIN_48,
                              INSAMP_OUTGAIN_1_94);
    }
    else if(!strcmp(command,S10))
    {
        time=10;
    }
    else if(!strcmp(command,S20))
    {
        time=20;
    }
    else if(!strcmp(command,S30))
    {
        time=30;
    }
    else if(!strcmp(command,S60))
    {
        time=60;
    }
    else if(!strcmp(command,S90))
    {
        time=90;
    }
    else if(!strcmp(command,S120))
    {
        time=120;
    }
    else if(!strcmp(command,S180))
    {
        time=180;
    }
    else if(!strcmp(command,S240))
    {
        time=240;
    }
    else if(!strcmp(command,S300))
    {
        time=300;
    }
    }
    UART_CmdReset();
}
if(run==1)
{
    while(DelSig_fIsDataAvailable()== 0);
    ADC_Output=DelSig_iGetDataClearFlag();
    UART_PutString(ftoa((float)ADC_Output,status));
    UART_CPutString(" ")

```

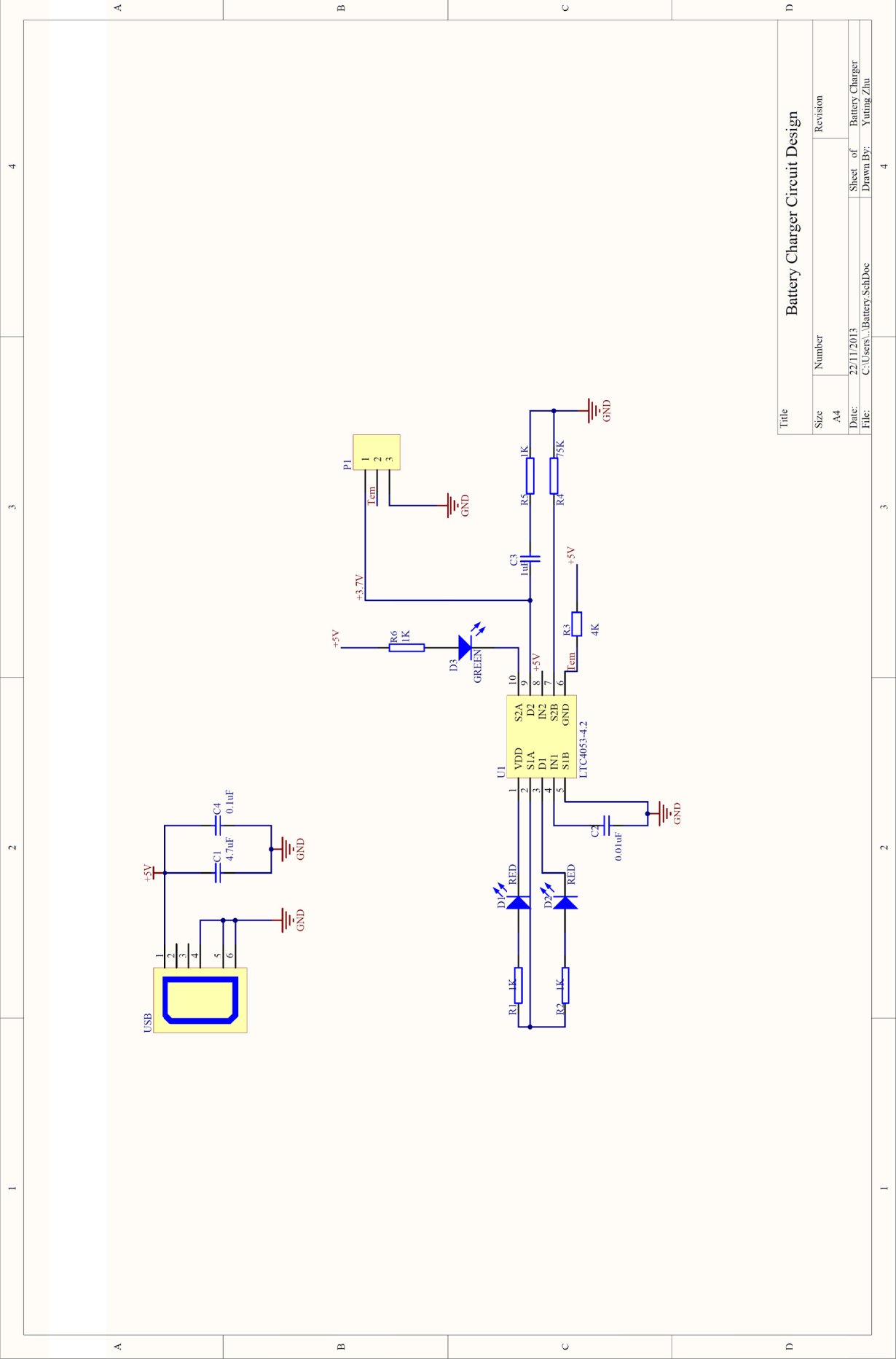
```
        }  
    }  
}  
  
void timecount(void)  
{  
    x++;  
    if(x==time)  
    {  
        stoppro();  
        run=0;  
        x=0;  
    }  
    return;  
}
```

Appendix H:

**Circuit Diagram for the WsEMG Electrode
Interface Node**

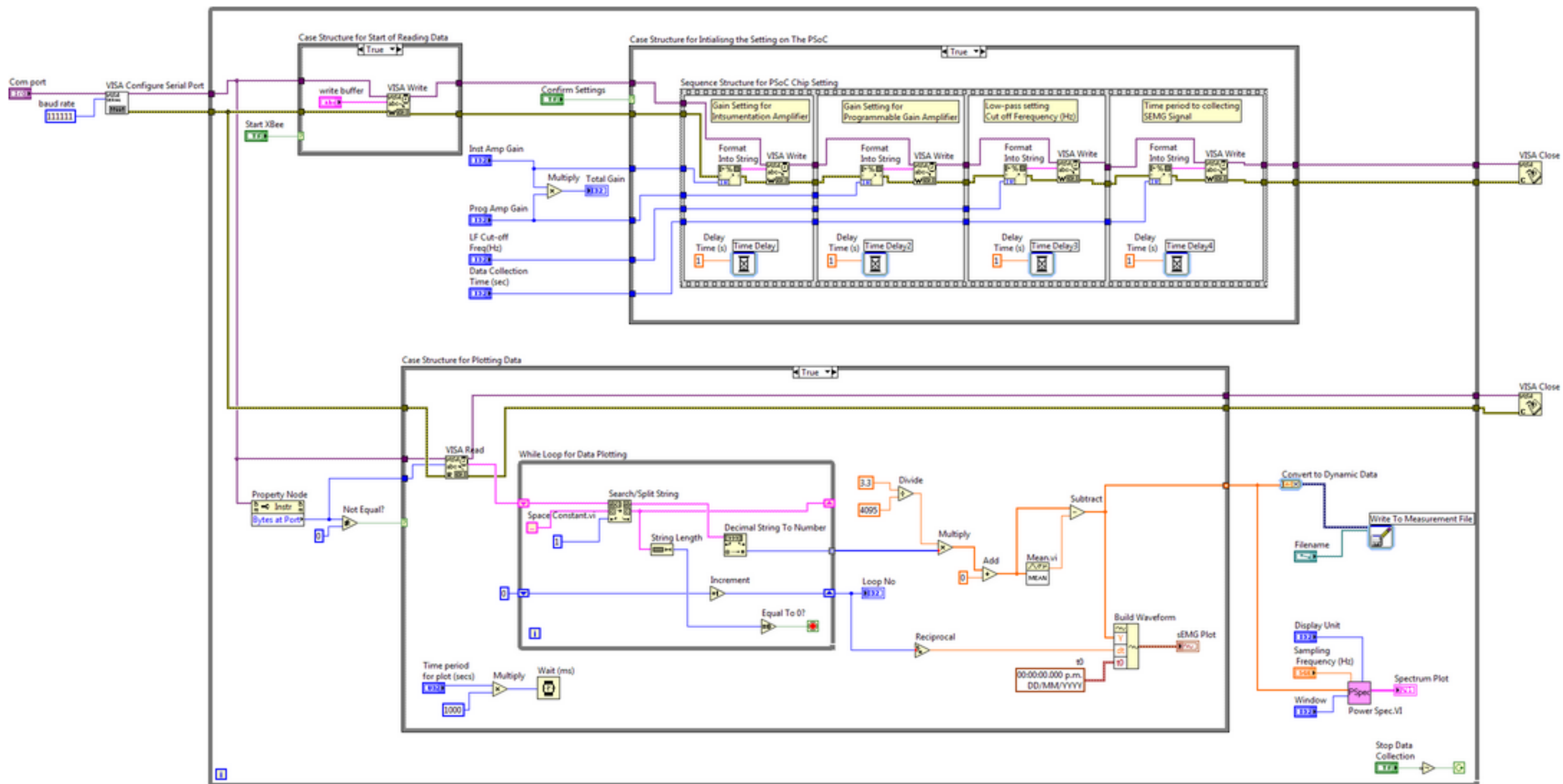
Appendix I:

**Circuit Diagram for Lithium-ion Polymer
Battery Charger**



Appendix J:

LabVIEW Block Diagram for Data Acquisition



Appendix K:

Ethics Approval



MEMORANDUM

Auckland University of Technology Ethics Committee (AUTEC)

To: Jeffrey Kilby
From: **Dr Rosemary Godbold** Executive Secretary, AUTEC
Date: 15 May 2012
Subject: Ethics Application Number 12/48 **Wireless electrodes for the collection of surface electromyography signals.**

Dear Jeffrey

Thank you for providing written evidence as requested. I am pleased to advise that it satisfies the points raised by the Auckland University of Technology Ethics Committee (AUTEC) at their meeting on 12 March 2012 and I have approved your ethics application. This delegated approval is made in accordance with section 5.3.2.3 of AUTEC's *Applying for Ethics Approval: Guidelines and Procedures* and is subject to endorsement at AUTEC's meeting on 28 May 2012.

Your ethics application is approved for a period of three years until 15 May 2015.

I advise that as part of the ethics approval process, you are required to submit the following to AUTEC:

- A brief annual progress report using form EA2, which is available online through <http://www.aut.ac.nz/research/research-ethics/ethics>. When necessary this form may also be used to request an extension of the approval at least one month prior to its expiry on 15 May 2015;
- A brief report on the status of the project using form EA3, which is available online through <http://www.aut.ac.nz/research/research-ethics/ethics>. This report is to be submitted either when the approval expires on 15 May 2015 or on completion of the project, whichever comes sooner;

It is a condition of approval that AUTEC is notified of any adverse events or if the research does not commence. AUTEC approval needs to be sought for any alteration to the research, including any alteration of or addition to any documents that are provided to participants. You are reminded that, as applicant, you are responsible for ensuring that research undertaken under this approval occurs within the parameters outlined in the approved application.

Please note that AUTEC grants ethical approval only. If you require management approval from an institution or organisation for your research, then you will need to make the arrangements necessary to obtain this.

To enable us to provide you with efficient service, we ask that you use the application number and study title in all written and verbal correspondence with us. Should you have any further enquiries regarding this matter, you are welcome to contact me by email at ethics@aut.ac.nz or by telephone on 921 9999 at extension 6902. Alternatively you may contact your AUTEC Faculty Representative (a list with contact details may be found in the Ethics Knowledge Base at <http://www.aut.ac.nz/research/research-ethics/ethics>).

On behalf of AUTEC and myself, I wish you success with your research and look forward to reading about it in your reports.

Yours sincerely

Dr Rosemary Godbold
Executive Secretary
Auckland University of Technology Ethics Committee

Cc: Yuting Zhu yuting.zhu@aut.ac.nz

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